

**The Egress of Fluid from the Brain via Arachnoid
Transport: Foundational Work for the Tissue Engineering of
the Arachnoid Granulation**

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Dedication

To my dearest boys,

Zeke and Nate...

I hope you never stop learning.

Abstract

The arachnoid tissue is a critical component for the removal of cerebrospinal fluid (CSF) and other substances. Failure results in hydrocephalus, increased intracranial pressure, and buildup of toxic materials in the brain. The purpose of this thesis is to establish a foundation for a biomimetic arachnoid construct. First, we characterized arachnoid cell transport in culture and on three-dimensional collagen scaffolds. Arachnoid cells were harvested from rat brainstems and cultured onto bilayered bovine collagen scaffolds. Cells exhibited arachnoid cell phenotype (positive for vimentin, desmoplakin, and cytokeratin), readily penetrated the collagen scaffold, and doubled approximately every 2–3 days. The transepithelial electrical resistance for a monolayer of cells was $160 \Omega \cdot \text{cm}^2$, and permeability of indigo carmine was $6.7 \pm 1.1 \times 10^{-6} \text{ cm/s}$. Hydraulic conductivity of the collagen construct was $6.39 \text{ mL/min/mmHg/cm}^2$. Because of practical limitations of primary culture which include slow growth, early senescence, and poor reproducibility, we created two immortalized rat arachnoid cell lines using retroviral gene transfer of SV40 large T antigen (SV40 LTA_g) either with or without human telomerase (hTERT). They stably expressed either SV40 LTA_g alone, or SV40 LTA_g and hTERT, and demonstrated high proliferative rate, contact inhibition at confluence, and stable expression of protein markers characteristic of native arachnoid cells for more than 160 passages. We subsequently used them to determine arachnoidal barrier properties and paracellular transport. Permeabilities of urea, mannitol, and inulin were $2.9 \pm 1.1 \times 10^{-6}$, $0.8 \pm .18 \times 10^{-6}$, and $1.0 \pm .29 \times 10^{-6} \text{ cm/s}$ respectively. Size differential permeability testing with dextran clarified the arachnoidal blood-CSF-barrier limit and established a rate of intracellular transport to be two orders of magnitude slower than paracellular transport in a polyester membrane diffusion chamber. The theoretical pore size for paracellular space was 11 \AA and the occupancy to length ratios were 0.8 and 0.72 cm^{-1} for urea and mannitol respectively. The monolayer permeability was not significantly different from an apical to basal direction or vice versa. Gap junction may have a role in barrier formation. Although up-regulation of claudin by dexamethasone did not significantly alter paracellular transport, increasing intracellular cAMP decreased mannitol permeability. Calcium modulated paracellular transport, but only selectively with the ion chelator, EDTA, and with disruption of intracellular stores. Without the neurovascular unit of the blood-brain-barrier, the blood-CSF-barrier at the arachnoid tissue is anatomically and physiologically different from the vascular based blood-brain-barrier. These studies provide a three dimensional architecture, a stable

cellular substrate, and baseline blood-CSF-barrier properties for the establishment of a viable bioartificial arachnoid shunt.

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List of Papers

Chapters 2 and 3 have been previously published in *Tissue Engineering Journal A*, and *Neuroscience* respectively. Chapter 4 is under review.

C. H. Lam, E. A. Hansen, and A. Hubel, "Arachnoid cells on culture plates and collagen scaffolds: phenotype and transport properties," *Tissue Engineering. Part A*, vol. 17, no. 13-14, pp. 1759-1766, Jul. 2011.

C. Janson, L. Romanova, E. Hansen, A. Hubel, and C. Lam, "Immortalization and functional characterization of rat arachnoid cell lines," *Neuroscience*, vol. 177, pp. 23-34, Mar. 2011.

C.H. Lam, E.A. Hansen, C. Janson, A. Bryan, A. Hubel, "The Characterization of Arachnoid Cell Transport: Paracellular transport and Blood CSF Barrier Formation of Arachnoid Cells," in review.

Chapter 1

Chapter 1: Background and Introduction

Chapter 1

The arachnoid

History of arachnoid physiology research

The recognition of the arachnoid granulation as an anatomic entity occurred during the Renaissance period in the 1500's and 1600's. While noted by Vesalius and Willis during this era, the granulation was not studied in detail until Pacchioni in 1705.[1] Its location adjacent to the sagittal sinus indicated to him an interfacial role for this structure. For his contribution, the granulation is sometimes referred to as a Pacchionian granulation.[2] Luschka in the 1800's correctly pointed out that the sagittal sinus has along its banks lacunes in which cerebral veins drain and which form outpockets with flat surfaces within the leaflets of the dura for arachnoid to protrude.[3] He was the first to recognize that granulations are the expanded versions of arachnoid villi, the former existing in the scale of millimeters and the latter, one tenth of that. In truth, the description villi and granulations are definitions along a continuum in terms of the size of these structures. This was expanded upon by Weed in 1914.[4] Weed also injected potassium ferrocyanide at low pressures into the CSF, and found that it collected in the granulations. It also collected to a lesser degree in the cord and lymphatics thereby discovering other important routes for cerebrospinal fluid (CSF) egress. He confirmed earlier works by Quincke who, using cinnabar postulated that the granulations may be important for the material removal.[5] He, Weed, Key, and Retzius were some of the earliest workers in the study of arachnoid transport.[6]

Harvey Cushing in 1901 realized that the pressure gradient variations within the vascular system demand a means for regulation of flow between it and the intracranial/intraspinal cavity.[7] One mechanism would be a valve, which would prevent extravasation of blood into the CSF space. Weed however has considered the granulations not as valves but blind diverticulum that were semi-permeable to fluid and dissolved substances; he could not explain the egress of particulate matters through the granulation as pointed out by Davson.[8] Not until 1961 did Welch and Friedman demonstrate that granulations indeed behaved much like valves. By using granulations from the African green monkey (*Cercopithecus aethiops sabaeus*), they showed that the villus is made of a series of interconnected tubes 4-12 micrometers in diameter at

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normal pressures. When the pressure is higher on the vascular side, these tubules collapse thereby shutting down flow.[9]

Quantitative measurements of material transport out of the brain began in the 1950's. Courtice and Simmonds in 1951 used labeled plasma protein injected into the cistern magna to trace CSF circulation in the cat. They found that about 4 hours later, 11-19% was in the bloodstream.[10] Simmonds used radioactive phosphate tagged to erythrocytes in the cisterna magna, which again appeared into the systemic circulation at a rate of 1% of injected dose per hour. He found that lymphatic ligation did not change the rate surmising that the arachnoid may play a dominant role [11]. Confirming Weed's ferrocyanide work, Key and Retzius found that some trypan blue injected into the CSF circulation ended in cervical lymph nodes in human specimens.[6] Sweet and Locksley placed lumbar subarachnoid, and bilateral lateral ventricular catheters in patients and found that radioactive potassium and chloride exchanged throughout the ventricular system, but albumin was lost primarily from the subarachnoid space hypothesizing that ions transferred differently than higher molecular weight material. [12] When Ishibashi in 1959 administered electrolytes and albumin into dogs, he found that the cerebrosubarachnoid route of egress was faster than the cerebroventricular or spinal subarachnoid route, presumably because this was closer downstream to the absorptive site.[13]

The demonstration of molecular transport in the 1950's was paralleled by particulate transport using similar experimental paradigms. In 1951, Adams and Pravirohardjo injected radioactive chromium-labeled RBC into the cistern magna of dogs. 48 hours later, 24% of intact RBC's were seen in the systemic circulation. The remainder was in the CSF, brain or predominantly, the arachnoid.[14] Welch and Pollay in 1961 utilized in vitro monkey villi and tested monkey erythrocytes (7.5 microns), goat erythrocyte (4 microns), yeast (3-6 microns), polystyrene microspheres (1.17-1.8 microns), and colloidal gold (.2-.3 microns) finding that these substances can traverse the arachnoid, but larger polystyrene microsphere in the range of 6.4-12.8 microns did not pass.[15]

Barrier studies classically involve the use of small molecular weight sugars, which presumably were transported mainly paracellularly. In the 1960's, Porckop, Schanker and Brodie placed microliter amounts of tracers (inulin, sucrose, dextran 40K, and mannitol) in the lateral ventricle

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and cisterns of the rabbit and found that 8.1 to 11.4% was left behind 6 hours later.[16] This suggested that bulk flow had a larger role than diffusion in the movement of these substances. Heisey et al. in 1962 measured inulin absorption and found that with increased pressure, bulk removal increased linearly.[17] When variable dextran weight was used by Davson in 1970, he found that changing the colloid osmotic pressure ten-fold did not result in any decrease in the flow rate. However, he determined that the more viscous the solution, the slower the flow rate. Furthermore, when he obstructed the villi with particulates such as kaolin, blood, or colloidal graphite, pressure increased with constant ventricular infusion experiments.[18]

The demonstration of particulate matter crossing the arachnoid granulation poses an apparent contradiction to the concept of blood CSF barrier. How does a barrier that permits only substances under a hundred kilodalton in size to enter, allow macroscopic debris to be removed? Up to the 1960's, the concept of the blood brain barrier (BBB) was simplistic, that it was formed from tight junctions between endothelial cells, and that substances either go through the cell or through the paracellular pathway. The latter is size limited depending on the how wide is the paracellular space.[19] The arachnoid granulation at the BCB also possesses endothelial cells. Alksne using EM found the endothelial layer overlying the granulation to be continuous.[20] The endothelial cell was therefore thought to be responsible for the barrier properties at the granulation. Furthermore, in 1965, Alksne and White found that the villi cells thinned with increased pressure and that vesicular numbers increased.[21] Alksne and Lovings (1972) therefore suggested that transport was energy consuming and therefore intracellular.[20] This could explain the apparent contradiction in which large particles may be admitted via vacuolization while an apparent size differentiated barrier still exists paracellularly. The study was the first cellular study with a semi-dynamic paradigm demonstrating morphologic changes of the arachnoid at varying pressure. Further evidence came about from Tripathi, who showed that at low pressure, the cells contracted with folds in the cell membrane manifested as microvilli, and with high pressure, vacuolization within the cells occurred.[22] High pressure morphologic change was addressed in 1973 and 1974 when Gomez, Potts, and others showed the cells and fibers in the arachnoid to be farther apart with widening of intercellular space at increased pressure in monkeys and sheep.[23] Cellular overlap decreased as pressure gradients increased. This suggested, for the first time, variation in the paracellular transport dependent

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on pressure. With increases in intracranial pressure, the arachnoid granulation expands, losing its lobules and becoming tense. Overlaps of neighboring endothelial cells become shorter, and the intercellular spaces, originally irregular and closely approximated, widen. Endothelial-lined tubules became visible. As the endothelium-lined tubules that extend into the granulation become distended, the endothelial cells show increased pinocytosis, and the stromal cellular and extracellular components become more separated. The microvilli covering the endothelial cells decrease in number and size, and the areas of apposition of adjacent endothelial cells were more irregular and sparse.[24]

More physiologic data began to appear in the 1970's. Labeled proteins injected into the CSF were found to be linearly secreted with respect to pressure into the blood. Resistance of flow is unaffected by colloid osmotic pressure of CSF.[25] Absorptive pathways of recently sacrificed dog approximate the normal living rate of CSF formation as measured as a pressure gradient between cisterna magna and sagittal sinus.[26] Both pieces of data suggest an important passive component to transport. Also, resistance of CSF outflow is relatively stable with changes in intracranial pressure in man, suggesting passive conduct of CSF similar to an electrical resistance model.[27] Based on clinical data using a constant-pressure, constant-infusion-rate test and reviewing data from other investigators, Albeck et al. calculated the overall outflow conductance of CSF to be from 0.08 to 0.13 cc/min·mmHg.[28]

The vesicular data indicates an intracellular as well as an extracellular component to material transport. It is likely that both mechanisms are utilized. Intracellular transport is complex, where molecular engines, transporters, and channels may all have roles. It has also been suggested that ingestion may take place in the arachnoid, blurring the boundary between transcellular transport and phagocytosis. Shabo in 1968 and 1969 showed that arachnoid cells in the villus core phagocytose both homogenized brain and peroxidase injected into the cisternal space complementing the plasma cells also seen in the arachnoid core. [29] More recently, Xin found that arachnoid cells themselves may present antigen and express basic HLA-DR.[30] Interspecies differences may compound the determinations of dominance of the various intracellular routes. Upton and Weller suggest that pinocytosis may be important in lower animals, but vacuoles may be more important in primates. Most however would agree

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that a combination of routes is at play in normal and pathologic states.[31] It therefore is clear that the role of arachnoid and the various egress pathways for CSF and substances it carries are complex.

Until cells could be separated in isolation, the exact roles of intra and extracellular pathways could not be studied in much detail. Frank was the first to establish primary arachnoid cultures (1983).[32] In 1985, Rutka et al. compared them to their tumoral counterparts. He also delineated the components of the extracellular matrix. [33] The matrix is complex and may contribute to barrier formation. In 2005, Holman et al. characterized the junctional proteins of cells *ex vivo*.[34] While cells have been cultured from arachnoid since the 1980's, this was the first study to determine the molecular components necessary for paracellular transport. Holman demonstrated the presence of connexin 43, desmoplakin 1 and 2, E-cadherin, and zonula occludin-1 in arachnoid. In 2006, Grzybowski used arachnoid cells on semipermeable membranes to determine the hydraulic conductivity on a monolayer.[35] She found the hydraulic conductivity in the B to A direction to be $4.52 \pm 0.43 \mu\text{l}/\text{min}$ per mmHg/cm^2 , and $0.29 \pm 0.16 \mu\text{l}/\text{min}$ per $\text{mm Hg}/\text{cm}^2$ from the A to B direction at an average transcellular pressure gradient of $3.33 \pm 0.16 \text{ mm Hg}$. While the direct relevance to the pressure gradient behavior physiologically on a membrane is questionable, it indicates that transport behavior of arachnoid cell may be directionally dependent. She also determined that the hydraulic conductivity is dependent on the pressure gradient. Holman found that when cells were perfused in the B to A direction, they manifested vacuoles, micropinocytotic vesicles, and extracellular cisternal spaces.[36] When perfused A to B, no large vacuoles were seen, and few extracellular spaces between cells were noted. Glimcher in 2008 [37] then perfused whole arachnoid granulation *ex vivo* to demonstrate what Welch et al. has done previously [15] using FITC polystyrenes spheres 0.1 to 2 micrometer in size. He showed tracers in all portions of the arachnoid granulation including the stem, core, and apex. The tracers grossly gravitate toward the arachnoid cap indicating a directional component to granulation mediated flow. However, the calculation of hydraulic conductivity is complicated by measurements of arachnoid granulation surface area (average area of perfused visible arachnoid granulation was 0.02082 cm^2 while the area of perfusion chamber was two order larger).

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Embryology of arachnoid

The behavior of the arachnoidal BCB cannot be explained completely by its ontogeny. The origin of its blood brain barrier counterpart, the vascular endothelial cell, is well established and its development is well characterized. The arachnoid's origin is more diverse and unknown.[38] It is likely the cells originate from endodermal, mesodermal, and ectodermal tissue despite its similar appearance in the cranial and spinal areas. Depending on the location, spinal and cranial, the contribution of the different primordia may be different. In humans, at stages 7-11, pre-arachnoid mesenchyme begins to form from the primitive streak, neural crest, prechordal plate, and neural tube. At stages 11 and 12, the mesenchyme begins to organize around the brain and spinal cord, first laterally in the brain, then in the basal and roof area. At stage 14, blood vessels enter the brain. When a cellular sheet intervenes between the cerebrum and the pial blood vessels, it is considered the pia mater, or the arachnoid that is directly adherent to the brain. Presumably, barrier formation commence at this stage. The leptomeningeal meshwork differentiates at stages 17 and 18 to be filled with liquid, which originates through the thin area membranacea of the fourth ventricular roof. This is the beginning of the cerebrospinal fluid (CSF) circulatory space and the future subarachnoid space. This primitive subarachnoid space spread caudally around the spinal cord and rostrally to the forebrain. In general, it tends to spread from ventral to dorsal. By stages 21-23, the process is complete with the space around the whole neural tube. At the external boundary of the leptomeningeal meshwork, a dural limiting layer begins to form. The dural limiting layer develops into a thin two dimensional sheet that later is recognized as the arachnoid membrane. Beyond this layer is the peripheral mesenchyme that forms the future dura mater. The transverse and sigmoid sinuses develop into the dura mater (stage 19), with the arachnoidal layer lies just under. The sinuses contain the vascular component of the arachnoidal BCB. One stage later, stage 20, the choroid plexus of the lateral ventricle is visible, which contribute to the CSF formation in the newly formed subarachnoid space. By 26 weeks, depressions form in the venous dural wall, which contain clusters of arachnoidal cells between the dural fibers. By 35 weeks, these become protrusions through the dura. From 39 weeks, the number of arachnoid villi increases. As an individual age, the size of the villi also increases to a visible size at which time it becomes a granulation. This evolution is likely pressure related rather than genetically governed. When

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subjected to insult, the villi degenerate and occlude. The description of granulation development and maturation underlines the changing physiology of this organ. Its site specificity, variable configuration, alteration with age, and diverse embryologic origin no doubt impact on the transport properties of the organ.

Anatomy of Arachnoid Tissue

Gross description

As noted into the embryology section, the layers making up the pachymeninges and leptomeninges occur late compared to the remainder of the neural structures. Yet all three layers are important for the support and encasement of the brain and spinal cord. These three layers are the dura mater, pia mater, and the arachnoid. The most clearly identified and most external is the dura mater, also known as the pachymeninges. It is situated adjacent to the bone, and is made of dense connective tissue. This layer forms the support on which the arachnoid granulations subside. The leptomeninges are made up of the pia mater and the arachnoid membranes, both of which are composed of identical cells. These two layers are thought to be of the same origin, the pia being closely adherent to the surface of the brain and spinal cord, and the arachnoid membrane, a paper thin structure with reticular fibers, extending to the pia in a web like (hence its namesake) fashion. Within the strands of the arachnoid lies the subarachnoid space, which is where the CSF circulates to be ultimately absorbed by various outflow pathways. At specific locations along the venous sinuses are granulations which allow the subarachnoid space to be in contact with the vascular system.

Anatomy of the arachnoid granulation

The arachnoid granulation is composed of a fibrous capsule, an arachnoid cell layer, a cap cell cluster and a central core. (Figure 1.1) The term villus is generally used for these protuberances that are too small to see macroscopically, while the term granulation is for grossly visible structures. In either case, it is divided into a narrow region called the pedicle and a more dilated portion called the body. The body is made of lobules, with solitary granulations tending to have fewer but larger lobules. The lobules are randomly distributed on the surface. In a newborn, the granulations are small and bullet shaped, but they are numerous. In an older individual, the granulations are fewer in number, but can be large reaching several millimeters

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in size. The fibrous capsule is often absent at the apical portion of the villus, leaving the arachnoid cell layer touching the endothelium-lined lumen of the lacuna or sinus directly. The cap cell cluster is a thickened layer of arachnoid cells, which can consist of an outer and inner zone, but also can be only one cell layer thick. The central core consists of arachnoid cells mixed with connective tissue fibers, and is in continuity with the subarachnoid space. Collagen fibers are of varied thickness, the largest and thickest being on the outside framework of the granulation while the thinnest are distributed internally similar to spider webs. The arachnoid cells contain larger number of intermediate filaments in the inner zone than the outer zone. Vimentin stain is positive for these cells, and on electron microscopy, intermediate filaments and desmosomal plaques are found to localize internally. The arachnoid cells have a variety of cell forms, intermediate filaments, and desmosome numbers depending on location.[39]

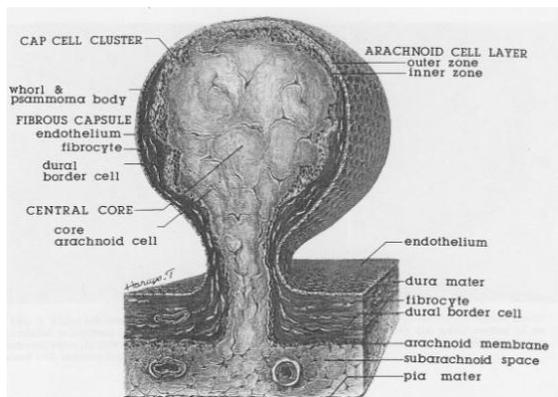


Figure 1.1: Arachnoid granulation . Drawing of a pedunculated arachnoid granulation showing the subarachnoid space, central core, and cap (from Kida et al. 1988). We have been able to tissue engineer the different components of the granulation and replicate its transport abilities.

The arachnoid tissue at the granulation structurally is well adapted for its role as the gateway for bulk flow from the intracranial cavity to the venous vascular system. Situated on the venous sinus, a constant flow of blood rushes by carrying substances passed onto its surface. It is pedunculated with a narrow waist, which serves as a valve preventing sudden breach in the vein leading to hemorrhage intracranially. Within the granulation, arachnoid exists in three forms: a flat two dimensional sheet that encase the granulation, a spider-like structure in the arachnoid

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core giving it form and at the same time porosity for material passage, and a densely packed arachnoid “cap” that may hold progenitor cells for future arachnoid cells.

The granulations exist in a number of locations, but most are along the superior sagittal sinus near the apex of the head. This has the greatest pressure gradient and therefore the fastest transport. Along the transverse sinus near the torcula and even around the sella tursica are some granulations as well. Sometimes, granulations are absent, in which case, lymphatics may play a substantial role in CSF transport.

Arachnoid granulations are ideal candidates for tissue engineering in many ways. The size of the granulations is in the order of millimeters. The individual cellular layers that make up a granulation are simple and not always present.[40] This suggests an extremely forgiving system. For some of these layers, i.e. endothelium, cell culture technology has been developed in the laboratory already. Finally, the rheology of CSF is similar to water, without the complicating contents of the blood. CSF is a fluid suitable for transport analysis with a body of literature on the bulk transport of CSF in the human already in existence.[41] This allows for benchmarks to compare natural constructs to the bioartificial product.

CSF pathway

Perhaps the most important substance transported by arachnoid tissue is CSF. The CSF is created from the parenchyma of the brain and from the secretion from the choroid plexus. The embryo likely first made CSF from the fluid generated metabolically, but as the neural structures become more complicated, the formation sites of CSF also becomes more diverse. Traditionally, the choroid plexus is thought to be an important source of CSF. Its rich blood supply and dedicated epithelial-like layer that intervenes between vasculature and the CSF is known to have not only a variety of transporters but also mechanisms for paracellular transport. The choroid plexus however is not the only source as early surgical ablation of the plexus only slowed CSF creation. The ependymal lining that covers the inner surface of the brain and the dural sleeves within the spine also are known to secrete CSF. The actual amount may vary depending on the degree of scarring and composition of the individual components, but about 80% is thought to originate from the choroid plexuses with approximately 90% of choroid plexus production is in

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the lateral ventricles. The actual output of CSF is not clearly defined, but estimated to be about 500cc/d in an adult.[42]

CSF

The composition of fluid that constitutes bulk flow varies slightly depending on where it is sampled. Grossly, CSF is clear harboring very few cells (0-5 lymphocytes or mononuclear cells per mm³, and no erythrocytes nor polymorphonuclear leukocytes (PMN)). With infections, this of course changes, and CSF may become viscous due to debris and PMNs becoming the consistency of pus. For the most part, the constituents are fairly uniform day to day with some variations depending on the age of the patient. Protein content varies from 20 -160 mg/dl, and glucose, 20-120 mg/dl. The remainder of the important CSF solutes is listed in Table 1.1. Some has regarded CSF to be similar to an ultrafiltrate of plasma except for a diminution in protein (6500 mg/100g to 25 mg/100g). In general, Na⁺, Cl⁻, Mg⁺⁺ content is higher and K⁺, Ca⁺⁺ and glucose is lower.

CSF	Units	CSF
Osmolarity	mOsm/L	295
H2O		99%
Sodium	mEq/L	138
Potassium	mEq/L	2.8
Chloride	mEq/L	119
Calcium	mEq/L	2.1
pCO2	mmHg	47
pH		7.33
pO2	mmHg	43
Glucose	Mg/dl	60
Lactate	mEq/L	1.6
Pyruvate	mEq/L	0.08
Lact:pyruva		26
Total	Mg/dl	35
Albumin	Mg/L	155
IgG	Mg/L	12.3

Table 1.1: Constituents in CSF of an adult (adapted from Greenberg[42])

Outflow

The CSF flows from the ventricles, first the lateral ventricles to the third, then via the Aqueduct of Sylvius into the fourth ventricle. There, it leaves via the Foramina of Luschka and Magendie to circulate around the spinal cord and the brain. The spinal cord and brain therefore are

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completely surrounded by CSF, which buffers, supports and cushions the CNS. The semisolid brain maintains its shape despite its 1500g weight because of its buoyancy, weighing only 50g when immersed. This reduces the acceleration and momentum the brain suffers during trauma. The CSF integrates the brain's various components geographically by transporting hormone and hormone-releasing factor. It removes waste from metabolism, breakdown products from trauma, and drug metabolites to be carried out of the nervous system. Neuro-endocrine substances, electrolytes, cellular waste, and protein pass into the fluid, diffusing in the subdural space, to be ultimately removed by arachnoid granulations and other points of egress (Figure 1.2).[43],[44] The CSF is then absorbed in various locations. The dominant location is thought to be the arachnoid granulations, but other sites include the root sleeves in the spine, the lymphatics along the paranasal region, and along the perivascular channels. (Figure 1.3) The contribution from each is variable, depending on the age and the specie. In macroscopic animals such as rats and sheep, the lymphatics have a substantial role.

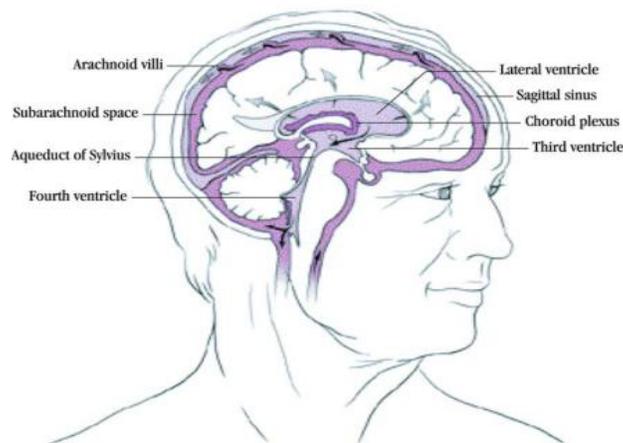


Figure 1.2: CSF flow

The brain is surrounded by CSF (purple) which cushions and facilitates transfer of material to and from the brain. It circulates from inside the ventricles to be absorbed into the arachnoid granulations.

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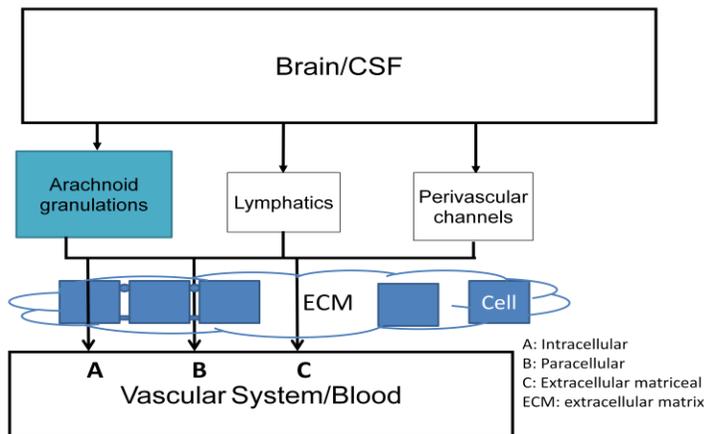


Figure 1.3: The direction of movement of blood and debris from the intracranial cavity to the vascular system.

Clinical Significance

Hydrocephalus

Among the most basic substances that the arachnoid transport is water. Cerebrospinal fluid is important for the function and maintenance of the brain, but, when there is a buildup of the fluid within the cranium, the clinical condition of hydrocephalus results. It can result from many neurologic conditions such as congenital anomalies, infections, neoplasms, trauma, and vascular disorders, and has an estimated prevalence of 1-1.5%. The incidence of congenital hydrocephalus alone is $\sim 0.9-3/1000$, making it one of the most common illnesses in a newborn. Approximately 60% of all hydrocephalus cases are in children. Currently, the vast majority of hydrocephalus is treated by a diversionary device consisting of a silicone tube with a valve that passes from the ventricle of the brain to the heart or the peritoneal cavity. Materials used in the valves are artificial, and typically are metal or corundum balls on springs, or silicone rubber in duckbill, slit, or miter configurations. Subjected to corrosion, infection, occasionally immunologic attack, the shunts have a high failure rate. An estimated 80,000 to 100,000 shunts are implanted each year in developed countries, leaving many more patients in undeveloped country without the benefit of shunting devices. [41] With the technology of shunting unchanged for over five decades, the complications rates and morbidity of having a shunt placed remains fairly constant and high, with a failure rate of around 50% over two years.[45] In the

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last fifteen years, development in biological materials and tissue engineering technologies has offered hope for regeneration of new physiologically active, absorptive tissue.[46]

Bioengineered shunts have not been developed yet, although there has been one attempt of using cultured cartilage to form a tube to mimic the current shunt technology; it however, has not been successful with rapid collapse of the tube after implantation.[47] Developing valve equivalents that drain into the venous system at the level of the arachnoid granulation would be the most anatomic and physiologic approach to the treatment of hydrocephalus.

Traumatic Brain injury (TBI) and the arachnoid

Cerebrospinal fluid is a central element for the physical support and chemical homeostasis of the entire central nervous system (CNS). Within the confines of the skull and spine, the soft brain and the cord would not be able to assume its natural conformation if not suspended in this fluid. As such, it buffers the brain from mechanical insults by dissipating the inertial forces delivered to the head, such as from blast injuries.[48],[49] Blast-related injuries numbers from the most recent conflicts in Iraq and Afghanistan may be as high as 320,000.[50] Because CSF surrounds the brain, it is also an important medium by which small molecules as well as particulate matter circulate along the neuraxis. With trauma, blood, blood products, and neural debris are washed into the CSF as well, which then is cleared from the CNS. Radiolabeled RBC studies determined that up to 76% of erythrocytes are trapped within arachnoid membranes.[51] The material load could be enormous. Lacerations of major blood vessels due to penetrating injury deposit massive quantities of blood into a skull of fixed volume (Figure 1.4).[41] Intracranial pressure (ICP) is then increased leading to decreased perfusion of the brain, distortion and herniation of the neural structures, and secondary injuries such as apoptosis and inflammation. The resultant enlargement of the fluid compartment due to blockage of the CSF pathway by mass effect of damaged brain or blood causes hydrocephalus, a medical condition that may result in severe brain damage and even death.[52] Therefore, diversion or clearance of the blood and debris becomes a major priority in the management of traumatic brain injury.



Figure 1.4: Blood washed into the CSF after trauma.
A victim of traumatic brain injury with ventriculostomy in place (arrow). This is an important, early, and universal treatment of traumatic brain injury. Note clear tubing from catheter to reservoir filled with blood (asterisk). Tremendous volumes of blood could be deposited into the CSF from trauma.

In the event of severe head injury, the single most important mean of controlling ICP is the diversion of CSF by an external ventriculostomy device (EVD), a plastic tube that diverts CSF into a bag at bedside (Figure 1.4). Current non-drainage treatments such as hypothermia do not remove waste or debris, which contribute to intracranial pressure due to the occupying space, incite inflammatory products, and deposit particulate matter obstructing CSF pathways. Despite its clear advantage over other treatment modalities, EVD's success in the removal of trauma induced detritus is limited. With a swollen brain, its surgical placement within the ventricle could be difficult. Blood clots and debris can plug the tubing. It is subject to breakage, disruption, and infection.[42] While this mainstay of neurosurgical treatment has been around for decades, no other therapy has improved on its efficacy. Therefore, an understanding of how the naturally occurring CSF "sink" drain could bring in new therapies.

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Traumatic brain injury releases of blood into the brain that results in a host of pathologic pathways, especially redox mechanisms (see review, Belcher et al., 2009).[53],[54] Our previous study and others have demonstrated the exquisite and selective sensitivity of the brain to redox factors that result from brain damage.[52],[52] Blood elimination therefore is a priority in the healing process. The marked ability for blood removal from the CSF has been known for almost 80 years.[55] Even when 8cc were injected into dogs, only 4% of injected blood remains in the CSF at 24 hours.[51] EM studies shows the lattice work of the arachnoid core to contain whole RBCs at 4 hours, and by day 3-5, RBCs have been seen within arachnoid cells by EM, in various stages of invagination.[51] Whether this is an indication of transcytosis or whether this is phagocytosis by the arachnoid is unclear. Argument for transcytosis is the demonstration of bulk material transfer in numerous vesicles, giant vesicles, and intracellular conduits in the arachnoid. Supportive evidence is also present on scanning EM which shows pores on the surface of arachnoid cells.[56],[57] Alksne et al. however argues that the arachnoid must serve the role of RBC break down instead. He finds that the endothelial layer on top of the arachnoid tissue to be yet another barrier that trauma debris must navigate before being transferred to the vascular system.[51] Others counter this argument stating that the endothelial layer is not always contiguous over the arachnoid.[58] Recently, Xin has shown that arachnoidal cells have some ability for antigen presentation and that basic HLA-DR is expressed in the cells.[30] The cells may play a role in the activation of T cells in the process of debris clearance[30], but suppurative findings in trauma is rare short of infection in the brain. Chopard has found that in the presence of blood, the paracellular space become wider.[59] Whether this is sufficient for macroscopic matter transfer is uncertain and will need to be investigated in the future. Clearly, the arachnoid's role in the trauma material removal is complex.

Barriers of the Brain and Neurotransport with Emphasis on the Arachnoid

Background

Historical Background: Molecular transport was discovered to be different in the brain compared to the other organs first by Paul Ehrlich in the 1880's.[60] He found that the Prussian blue injected the systemic circulation did not stain the brain while the other organs did. His original thought was that the brain does not have the same affinity for the dye compared to the

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rest of the body. However, when his pupil, Edwin Goldman injected Trypan blue into the CSF, the remainder of the body was not stained, suggesting that more likely there exists a barrier between the brain and the rest of the body.[61] This was further validated when Lewandowsky injected neurotoxic agents either in the vascular system or the brain, and found that only when directly injected into the brain did the agents have an effect. Lewandowsky first coined the term “blood brain barrier” to describe this phenomenon.[62] In the 1940’s, this barrier was found to be tunable by means of osmotic disruption.[63] The complexity of the blood brain barrier became more apparent in the 1960’s, when Crone et al. discovered that transport into the CNS involves multiple pathways including active transport in addition to passive diffusion.[64] In 1967, Reese and Karnovsky using high definition electron microscopy, studied the movement of horseradish peroxidase and found that the endothelial cells of the brain is marked different than the heart and muscle in that its tight junctions were much more closely knit and were the main barrier to molecular transport.[65] This is however not the case of all species. In elasmobranch fish and some invertebrates, the astrocytic foot processes is responsible for the separation of the brain from the remainder of the body.[66] In fact, in the 1960’s, it became apparent that at least four different kinds of cells in humans may be responsible for the differential transport behavior.

Architecture of the BBB and BCB: The three dominant cells existing at the barrier junction are the pericytes, astrocytes, and endothelial cells in the vasculature. Perivascular macrophages and nerve terminals are involved as well although to a lesser degree. The ratio of pericyte to endothelial cells is about 1 to 3. [67] Approximately 99% of the abluminal surface of the endothelial cells is invested by astrocytic foot process. Only about 20nm exists between the foot processes and the endothelial cell.[68] Perivascular macrophages however have been found within this space and expanding this space. The role of nerve endings most likely has to do with modulation of the barrier rather than being a part of the physical barrier. [67]

In contrast to the BBB, the BCB at the arachnoid granulation is rather simple. The vascular endothelial layer covers the granulation, albeit at times incompletely. Below is the subdural space. Abutting the endothelial layer is the arachnoid cap made up of a single cell type.[39] This construct has two barriers: the first at the endothelial layer and the second at the arachnoid

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layer. Dye injected either from below or above the endothelial layer could be restricted.[40] The contributions of both layers are probably important for barrier formation. However, during the early period of arachnoidal research, this was not clear. Alksne and colleagues used TEM and SEM did not demonstrate discontinuity of endothelium at the granulation [51], although, others have shown areas bare of endothelium along the lining [69]. Others have not only demonstrated breakages besides the endothelial cells, but within the cell were interendothelial clefts.[5] These were likely large vesicles having fusing together into a conduit. In the early 1970's it became clear that the endothelial layer is dynamic; Gomez demonstrated intercellular clefts to open with increased fluid pressures in sheep.[70]

Areas of the brain without endothelial cell barriers include the circumventricular organ, choroid plexus, and the retina. At the circumventricular organ, fenestrated capillaries have closely opposed to special ependymal cells with a network of loose tight junctions.[71] In the choroid plexus, cuboidal epithelium lines the surface also with contain special tight junctions.[44] In the retina, the blood vessels are fenestrated at the choroidea, and the barrier is made up of the retinal pigment epithelium.[67] These specialized areas do not have the same barrier capacity as the brain vasculature.

Microscopic architecture: The explanation for the selective isolation of the central nervous system originally was thought to be due to the small extracellular spaces resulting in tightly packed cells in the brain. This however cannot explain the rapid transport that occurs between the CSF and the rest of the CNS. Later when the tight junction in endothelial cells were found using freeze fracture techniques, its complexity and woven appearance underlie their importance in prevention of rapid transport. Freeze fracture demonstrated not only the strands, but also particles within the inner (P-face) and outer (E-face) lipid leaflet of bilayer membranes in the tight junction that fasten the strands together. From the P-face, a network of strands emerge leaving grooves in the E face. The number of strands in tight junctions is related to transcellular electrical resistance logarithmically.[72] Tight junctions have integral membrane proteins occludin and the more recently discovered family, claudin. Ig-superfamily junction-adhesion molecules of the JAM group and ESAM (endothelial cell-selective adhesion molecules) are also located at tight junctions. First-order adaptor proteins are those that are directly

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associated with integral tight junction proteins via PDZ domains. These include ZO-1, ZO-2, and ZO-3. Second-order adaptors are indirectly associated with the integral proteins. These include cingulin and cingulin-related protein. The control of tight junction is under various cascades including G-proteins, regulators of G-protein signaling and small GTPases.[73]

Paracellular machinery – tight junctions and other junctional structures

Among the earliest of the tight junctional transmembrane molecules discovered is occludin. Occludin was first found in chicken liver[74], and it shows wide interspecies variability except for the carboxy terminal. This ZO-1 binding domain is the most conserved region and links occludin to the cytoskeleton via its alpha-helical coiled structure.[75] Transepithelial resistance in large and small intestines is not altered in occludin-deficient mice, but the animals are more prone to chronic inflammation and hyperplasia of the gastric epithelium, calcifications in the brain and brain vessels, among other deficits.[76] Occludin is not needed for the formation of junctional strands, and posttranslational modifications such as phosphorylation of its cytoplasmic domains or ubiquitin-ligase binding may be important for junctional regulation.[76] Occludin in aortic endothelium is reduced by shear stress ($100 \mu\text{N}\cdot\text{cm}^{-2}$) and phosphorylation could be attenuated by dibutyryl cAMP.[77]

Claudins are similar to occludin in that it has four transmembrane domains, but it does not share any sequence homology to occludin. Again first identified in chicken, the family at present contains more than 20 members.[78],[79] Claudin is most likely responsible for the regulation of paracellular permeability by formation of a variety of homotypic and heterotypic pairing of strands. Ion selectivity is achieved through selective combination of distinct claudins and is organ specific. Claudin-5 and claudin-16 for example is in endothelial cells, stomach and intestinal surface cells while claudin-16 is in the thick ascending limb of Henle.[80],[81],[82] Occludin is associated with formation of short strands, but claudin is associated with long branched strands in the tight junction seen on EM.[83] Transfection of MDCK cells with claudin-1 increased TEER about 4 times with resultant decreased paracellular flux. Transfecting MDCKI cells (normally high TEER expressing claudin-1 and -4) with claudin-2 resulted in reduced resistance similarly to MDCKII cells.[84] Claudin-4 was formerly known as Clostridium

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perfringens enterotoxin receptor (CPE-R).[85] Brain endothelial cells contain claudin-1, -3, -5, and -12.[67]

Immunoglobulin-like proteins at the tight junctions are called junctional adhesion molecules (JAM). They have homotypic cell-cell contacts and appear to be involved in calcium mediated modulation of tight junction function.[86] They may also have a role in regulating leukocyte-endothelial cell interaction, although leukocyte diapedesis may follow a transcellular route called emperipolesis instead.[87] Other Ig superfamily members at tight junction include the coxsackie and adenovirus receptor (ECAR) endothelial cell-selective adhesion molecule (ESAM), JAM-4, and adenovirus receptor-like membrane protein (CLMP). They share with JAM-A, -B, and -C, two Ig-like domains.[67] These associate with other tight junctional components to make up cytoplasmic “plaque”. ZO-1, a 220-kDa phosphoprotein was the first to be identified at the tight junction. Others include adaptors, proteins with multiple protein-protein interaction domains such as Sh-3 domains, guanylate kinase (GUK) domains, and PDZ domains. These adaptor proteins include members of the membrane-associated guanylate kinase (MAGUK), membrane-associated guanylate kinase with an inverted orientation of protein-protein interaction domains (MAGI), and proteins with one or several PDZ domains families (ZO-1,-2,-3, MAGI-1,-2,-3, PAR-3,-6, MUPP1). By juxtaposing plaque proteins, these adaptor proteins organize the regulatory and signaling protein important for the tight junctions such as GTPase, their regulators, and the transcriptional regulator ZP-1 associated nucleic acid binding protein (ZONAB). [67]

Located at the apical end of the cell, tight junctions are capable of forming a continuous band around cells thereby preventing easy passage.[88] Located nearer the base are the adherens junctions and the gap junctions. Previously thought of as spot attachments, adherens junctions may also encircle cells (zonula adherens). Spots of attachments are known as adhesion plaques.[89] Adherens junctions are protein complexes which are linked to the actin cytoskeleton via its cytoplasmic face. Composed of cadherins, p120, beta-catenin and alpha-catenin, adherens junctions may mediate actin polymerization and maintain the actin contractile ring.[90] Gap junctions also join adjacent cells but have the additional role of forming intercellular channels that allow various molecules and ions to pass between them. Made of two connexin hemichannels, gap junctions permit electrical coupling to occur as well.

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In vertebrates the hemichannels are primarily homo- or hetero-hexamers of connexin. Each connexin protein has four transmembrane domains, and six connexins make up one hemichannel (connexin). Hundreds of gap junction channels make up the gap junction macromolecular complex.[91] The intercellular space at the gap junction is 4 nm, not only connecting and aligning the cells, but also tack welding the cells together and narrowing the intercellular space.[92]

Intracellular mechanisms - Vesicles and Vacuoles

As previously mentioned, the paracellular spaces in arachnoid open with increasing pressure, but Tripathi also demonstrated that pinocytosis increases with increased pressure.[5] More recently, Holman showed that pinocytosis occurred with vesicular size of about 1 micron in ex vivo cultures.[36] Tripathi in the late 1960's also showed large intracellular vacuoles, which could account for an additional pathway for particulate removal from the CSF.[1] The vacuoles have been seen on EM to convert to large pores on the apical surface of cells.

Intracellular mechanisms - Molecular machinery

The physiology of intracellular transport is not addressed in the thesis. However, it is important in the overall description of movement in and out of the brain. Part of the definition of the BBB is reduced ability of lipophobic material into pass thru the barrier. This is in part no different that epithelial layers in many other locations in the body. Lipid solubility may be characterized by octanol/water partition coefficient, charge and molecular size.[93] The importance of transmembrane channels that facilitate and bypass the lipid barrier continues to evolve. Transport proteins for specific molecules such as ions, glucose, and amino acids have been known for decades. Knowledge concerning other specific receptors such as the ABC proteins for the transport of medications (antiepileptics and chemotherapeutics) into the brain continues to evolve.[94] Receptors also mediate transport for critical molecular endocytosis. Materials transferred by this route include insulin and transferrin. For water, multiple members in the aquaporin family mediate the movement of water through the lipid layer.

Transcellular transport is mediated by two main systems: caveolae [95] and clathrin-coated pits [96]. Caveolae may be importance in signal transduction and docking sites for glycolipids and glycosylphosphatidylinositol-linked proteins. Insulin, albumin, ceruloplasmin, interleukin-1, and

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high density lipids (HDL) have caveolae receptors. Clathrin is important for the formation of coated vesicles. First isolated in 1975, it has a triskelion shape that interacts forming a polyhedral lattice surrounding the vesicle. Vesicles may transfer nutrients, import receptors and clean up debris. Chains of vesicles can form to become channels transgressing the entire cell. These transcellular tubules permit direct connections between the two sides of a cell.

The arachnoid cell

Leptomeningeal cultures

A large body of literature exists for dural cultures because of interest in meningeal tumorigenesis, but relatively few reports exist for leptomeningeal cultures.[97] There has been some interest in these cells' ability to secrete insulin-like growth factors, IGF binding protein and other extracellular proteins because of their role in meningioma formation.[98] While organotypic cultures of leptomeninges have been possible since 1975,[99] the initial description of pure leptomeningeal cell culture was not until 1983.[32] Frank demonstrated that these cells are robust, and could be even harvested from autopsy specimens. The cells grew readily from tissue fragments forming colonies within a few days. By using an enriched medium of Eagle's minimum essential medium containing nonessential amino acids, glutamine, gentamicin, and 10% fibronectin-free fetal calf serum, colonies were obtained from incubation at 37 degrees in a humidified atmosphere (95% air and 5% CO₂). Confluence is reached by 14-21 days. During the exponential phase of growth (subconfluence), the cells swirl broadly, and are bipolar with relatively large, rounded central nuclei with generous cytoplasm. The cytoplasmic edges tended to be curvilinear. Coarse streaming of cells into gentle arcs from colonies was seen. At confluence the cells no longer are bipolar and became homogeneously flat and polygonal. The terminal cell density in early passages was $3-5 \times 10^4$ cells/cm². There was no crowding compared with fibroblast cultures (density $1-2 \times 10^5$ cells/cm²). Doubling time in early passage was rapid (<24 hours). Trypsinization did not alter morphological features, but by passages five to seven, signs of senescence were apparent (increased cytoplasmic:nuclear ratio, cytoplasmic vesiculations, giant and often multinucleated cells). No cell cultures were viable after 15 passages, but by increasing intervals between passages, culture time is prolonged.

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Detection of the cells could be done morphologically and immunohistochemically. Clinical arachnoid specimen is identified by epithelial membrane antigen (EMA), which is positive also in arachnoid cyst, meningiomas and arachnoid rests.[100] Extracellular matrix from these cells stained positively for fibronectin, laminin, collagen type IV, and procollagen type III. Fibronectin and procollagen type II are particularly present in dense, granular focal plaques, with long thick fibrils forming a loose meshwork while laminin and collagen type IV deposited as much finer focal plaques. Electron microscopy of leptomeningeal cultures shows interdigitation of cell membranes and invagination of cytoplasm into nucleus. Specialized intercellular junctions such as gap junctions and desmosomes were also seen.[33] Cytoskeleton is formed by intermediate filaments (tonofilaments and monofilaments), and fine granular and filamentous basement membrane-like material is found in the extracellular spaces between cells. Probably the most important marker is cytokeratin positivity because of the similarity of arachnoid cells morphologically to fibroblast (cytokeratin negative).

The arachnoid barrier

Until recently, almost all knowledge gleaned from the blood CSF barrier (BCB) is derived from study of the choroid plexus, ependyma and circumventricular organs.[101] Paracellular diffusion, while restricted by tight junctions, is less tight than the BBB, and pinocytosis/exocytosis have been seen as a low-capacity means of transport at that location. While important as part of the CSF circulatory pathway though, these areas are the “source” of the CSF. Knowledge gained from this substrate does not shed light on the downstream border cells, the predominant form of which is the arachnoid. Clearance of the brain/CSF occurs at the “sink”, and only in the last several years have some its characteristics been discovered.[102]

Paracellular and Intracellular transport at the arachnoid station

The arachnoid “sink”, similar to most boundary cells has two main routes for egress, the paracellular and intracellular routes. It is uncertain as to the method by which arachnoid cells remove substances, but likely includes both depending on the molecular or particulate characteristics. Paracellular transport classically has defined the barrier property characteristic of brain barriers. Paracellular pathways for transport are influenced by the presence of tight junctions, zonula adherens, desmosomes and gap junctions. Tight junctions located near the

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apical portions of the cellular apposition play perhaps the most important role as it forms a continuous belt around the cell and are subject to a variety of mechanisms for control.[73]

Arachnoid cells stain positively for ZO-1 and occludin particularly around the periphery.

Desmosomal junctions are seen on electron micrographs of cultured cells, and the resistance to pressure relationship in a primary cell monolayer model appears linear. Lucifer yellow, a paracellular pathway marker, has a permeability of $7.19 \times 10^{-6} \text{ cm} \cdot \text{s}^{-1}$. [36] In our laboratory, we have developed monolayers of arachnoid cells with transepithelial electrical resistances (TEER) similar to MDCK type II cells, which is an established model of BBB. We show molecular weight disparity in arachnoid transport using FITC-dextran, which is similar to the BBB as well. These findings are indicative of a substantive role of paracellular transport in our model.

Intracellular transport has been studied in arachnoid cells primarily using electron microscopy (EM). Increased numbers of vesicles, giant vesicles and even transcellular tubular structures have been seen especially in conditions when pressure gradients such as during trauma are high across the tissue.[70] Crude ingestion experiments indicate that vesicles 1 μm in diameter form when cells are subjected to perfusate containing ruthenium red.[36] Penetration however was limited to inside the cell without further transport. Permeability values for MRI based computer modeling and in vitro monolayer models were similar, which confounds the finding given that the three dimensional complex architecture of arachnoid granulations is markedly dissimilar to a monolayer of cell.[103] A potential explanation is that the arachnoid functions in a phagocytic role rather than transcytotic transport role, which may be the case in the setting of traumatic brain injury.[30] Therefore, it is crucial detailed information concerning the intracellular transport for the arachnoid cell be obtained.

Tissue Engineering of CNS for Transport

Background neural tissue engineering

Neural tissue engineering in many ways has paralleled tissue engineering in other parts of the body. Scaffolds and cells native to the central nervous system are amenable to manipulation and duplication from the genetic to organ level. Gene therapy, immortalized cell lines, collagen and biopolymer scaffolds are areas of intense study in both the central and the peripheral nervous system. A central difficulty arising from the central nervous system is the exquisite

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dependency of function to localization. Unlike other organs where one area may be similar to another, in the brain and spinal cord, even micrometer geographic differences may subserve a totally different function. This thesis attempts to sidestep this issue by applying tissue engineering techniques to other tissues in the brain in which this focal localization specialization is not present. One of these areas is the arachnoidal tissue, which despite its embryologic diversity as seen in Chapter 1 is relatively uniform in appearance and function throughout the central nervous system.

Neural tissue engineering for CSF transport

While the study of arachnoidal cells and their extracellular matrix has been ongoing for several decades, application of tissue engineering techniques to arachnoid tissue is limited. Only one previous attempt has been used to culture arachnoid cells onto scaffold. This recent work used primary cells on a non-woven poly(ethylene terephthalate)(PET) scaffold.[104] The results were encouraging in that cells remained metabolically active and multiplied. Physiologic studies however difficult to interpret as Lucifer Yellow permeability and hydraulic conductivity of the constructs were similar between 2D and 3D architectures. Furthermore, the felt-like material does not recapitulate the native architecture of the arachnoid. It was clear though that these cells formed junctional proteins responsible for barrier capability and paracellular transport.

Another tissue engineering endeavor for CSF diversion was undertaken to treat hydrocephalus. Hydrocephalus is a major medical condition resulting from CSF drainage blockage. Lee et al. attempted to mimic not a natural product but a manmade device, the ventricular shunt, using tissue engineering techniques.[47] This attempt was to create a conduit similar to current silastic tubing that serves as an extraneous alternative detour for CSF to escape from the brain. The location of the device is between the ventricular and subarachnoid space, which is typically how CSF flows (via a series of ventricles and aqueducts). Because of the natural tendency for conduits to collapse, chondrocytes-seeded polyglycolic acid tubes coated with polylactic glycolic acid (PGLA) implants were used. The survival of the device was short lived and silastic tubing had to be temporarily substituted at the time of shunt insertion due to premature device collapse.

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As evident from the previous attempt, the scaffold for support of arachnoid cells is critical for the creation of a bioartificial arachnoid shunt. It has to be physically strong enough to provide for cell attachment as well as tolerate hydrodynamic forces until the cells can lay down their own extracellular matrix. Intracranial pressures typically are 8 to 12 cm of H₂O, but can exceed 100 torrs with Valsalva maneuver transiently. While venous side pressure reflects roughly right-sided atrial cardiac pressures maximally, superior sagittal sinus pressure typically is close to atmospheric in the upright position. The shape of the granulation tissue equivalent therefore has to be designed to accommodate these conditions. Collagen was chosen as the structural element because it is a well-known contributor to the tri-dimensional architecture of the arachnoid granulation.[105] The fibers have been found as thick bundles in the capsular extension of the meninges, and as thin "spider webs" (sic. arachnoid) in the inner frameworks of the granulation. Arachnoid cell cultures are known to lay down extracellular matrix in one week; therefore the scaffold must last at least this length of time. Current techniques of strengthening collagen scaffolds include increasing crosslinking of the collagen fibers. Aldehydes have been used, but they have a tendency to be poisonous to cells in culture. Ultraviolet light exposure has been successfully done on scaffold built with collagen solution concentration under 1%.[46] This is the technique we utilize. Ultimately, the scaffold should promote cell survival, enable signaling, and be conducive to extracellular matrix formation.

The scaffold in the intracranial environment should have other characteristics for optimum function. It must be thin so that migration of the cell need not to be extensive, and the cerebrospinal fluid should be able to enter the granulation without much impedance (target hydraulic conductance of 0.8-0.13 cc/min·torr). The scaffold should have one membranous surface such that the arachnoid cell migration is delimited. This skin of collagen allows the cells to be confluent such that the cerebrospinal fluid blood barrier can develop. At the same time, an open porous surface on the opposite side is needed for the cells to migrate in. Our porous bilayered scaffold is not unique. Glowacki et al. have been able to create this geometry in her laboratory as a method for delivering bone marrow proteins to cell cultures.[106] Similar to us, their pore structure in the collagen mimics the size and geometry to that of the inner core of a granulation. To extend this work, molds would be needed to contour the scaffold in a shape similar to a granulation macroscopically before seeding with arachnoid cells. The scaffold must

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be conducive for lamination to meninges such that eventually, the shunt could be integrated into the body. Finally, the outer layer of the scaffold also has to be permissive for covering by endothelial cells so that full integration into the venous sinus may occur.

The ideal tissue engineered arachnoid granulation should mimic the natural tissue as much as possible. Its biomechanical and physiologic properties, shape, and size, especially within the intracranial cavity with its limited space, are important factors in its design. This thesis will attempt to lay the foundation for the creation of optimal scaffolds and cellular substrate with characteristics moving toward those goals.

Chapter 2: Arachnoid Cells on Culture Plates and Collagen Scaffolds:

Phenotype and Transport Properties

Development of a Viable Three Dimensional Arachnoid Construct

The behavior of arachnoidal cells ex vivo has been studied since the 1980's. Outgrowth from primary cell cultures has been characterized as well as basic tabulations of extracellular matrix composition. More recently, the transport of selected tracers have also been the cells as a monolayer has been reported. Among the biologic architecture besides the two dimensional monolayer of the arachnoid tissue is a porous reticulated central core within the arachnoid granulation. With pore size around 100 microns, the core filters macroscopic particles and buttresses the cap and endothelial lining. It distends in response to intracranial pressure. Previously, one other attempt at mimicking this structure has succeeded in maintaining the cells in a three dimensional culture condition. However, the nonweaved matrix was artificial and did not duplicate the collagenous supportive structure underlying the cells. That paper however demonstrated hydraulic permeabilities within reasonable ranges may be arrived at using tissue engineering techniques. The following paper describes how primary rat arachnoid cells may populate a collagen scaffold, duplicate biologic equivalents in terms of three dimensional architecture, and maintain physiologic characteristics that in the future lead to the development of a tissue engineered arachnoidal shunt.

The work is carried out by Cornelius Lam and Eric Hansen under the guidance of Allison Hubel.

The paper is written by Cornelius Lam.

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Introduction

Hydrocephalus is a medical condition that results from blockage of cerebrospinal fluid (CSF) flow from the brain to the vascular system. The estimated prevalence of this condition is 1%–1.5%, with the incidence of congenital hydrocephalus at 0.02%–0.35%.[42] This is variable depending on geography and the underlying disease. If left untreated, this condition may result in severe brain damage and even death. Conventional methods of treating hydrocephalus involve the surgical insertion of bypass tubes to facilitate draining of CSF.[41] Unfortunately, complications and failure rates are high for this type of approach. The complication rate for the first year in the pediatric population is about 17%, and by 2 years, almost 50% of all shunts fail.[45] The arachnoid granulation is traditionally thought to be the primary route for CSF drainage.[31] Abutting the major draining veins of the brain and integrating into the walls of the superior sagittal sinus, the arachnoid granulation resides at the interface between the intradural space and the venous vasculature. Therefore, short of a mechanical blockage of CSF in the intradural space, failure of the arachnoid granulation is thought to be one of the primary causes of hydrocephalus.

The arachnoid granulation consists primarily of arachnoid cells with an endothelial cell layer. Within the granulation, the arachnoid cells are organized in two distinct layers.[39] The first is an arachnoid cap made up of tightly packed arachnoid cells several cell layers thick. Below is a porous core several millimeters thick that is mainly collagen extracellular matrix with a sparse population of arachnoid cells. These two layers are contiguous with the arachnoidal membrane that covers the central nervous system. Another arachnoidal layer, the pia, is tightly adherent to the brain.[39] Because they are anatomically more accessible and surgically more easily manipulated, cells here serve as a ready source for harvesting. Between the pia and the arachnoid membrane are sparse strands also made up of arachnoid tissue. The strands connecting the more superficial arachnoid membrane to the pia form a three-dimensional (3D) web-like network (hence the name arachnoid). This space between the two arachnoidal layers is the subarachnoid space in which the CSF circulates. The arachnoid granulation inhibits large molecules from entering into the CSF space while allowing small molecules such as water to pass.[107] The complete role of the arachnoid cells in the flow of CSF is unknown despite over

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100 years of study,[107] and only recently has the transport of arachnoid granulation in isolation been explored.[37]

Previous studies attempting to understand the function/ dysfunction of the arachnoid granulation have been limited.[104],[36] These studies used arachnoid cells obtained from human donors and characterized phenotype and permeability of cells cultured on synthetic matrices (nonwoven poly[ethylene terephthalate] [PET] and cell culture inserts). These studies demonstrated that arachnoid cells from humans can be cultured outside the body and that arachnoid cells cultured *ex vivo* exhibit a directionality of water flow (i.e., hydraulic permeability differs based on the direction of flow). These studies are important in establishing the ability to culture arachnoid cells *in vitro* and the basic transport characteristics of cell monolayers. The previous studies do little to recapitulate the native arachnoid granulation. The objective therefore of this investigation is to culture arachnoid cells in a 3D collagen matrix, characterize their behavior, and compare it to that observed in two-dimensional (2D) culture. The development of an appropriate *in vitro* culture model for the arachnoid granulation can be used to elucidate the function of the granulation and its role in hydrocephalus, to evaluate new therapies to treat the disorder, and ultimately to aid in the development of a fully tissue-engineered arachnoid granulation.

Materials and Methods

Cell isolation

Arachnoid cells were isolated from 19-day-old rats (*Rattus norvegicus*) with approval from the Minneapolis Veterans Administration Medical Center and University of Minnesota animal care committees. Animals were anesthetized before sacrifice and the pia-arachnoid tissue was harvested from the anterior portion of the brainstem using microsurgical techniques. The tissue was washed three times in phosphate buffered saline (PBS), cleared of extraneous tissue, and chopped into 1X1mm² pieces.

Tissue fragments were incubated at 37°C in humidified atmosphere of 95% air and 5% carbon dioxide in a culture media containing Eagle's essential medium with 10% fetal bovine serum (Remel Inc.), nonessential amino acids (Sigma Aldrich), glutamine (BioWhittaker Inc.),

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streptomycin, and penicillin (Gibco Invitrogen Corp.) at 10mL/cc each; the medium was changed twice per week. Cyclic AMP (cAMP) (2%; Sigma Aldrich) was added to the culture media for a limited number of cultures. Within 2–3 days cells were seen growing out of the dissected tissue, and after 7–10 days the cells became confluent. They were passaged following trypsinization with a 1:2 dilution of 0.05% trypsin-0.02% EDTA (Gibco Invitrogen Corp.) mixed with PBS. Cells were grown on Nunclon 6-well plastic plates (Thermo Scientific, Inc., 9.34 cm² well surface area). Cells could not be passaged beyond passage 9–10, and most experiments used cells from passage 3 or 4.

The phenotype of the cells isolated from the tissue was confirmed using immunohistology. The cells stained positively for cytokeratin and colocalized for desmoplakin and vimentin; these markers are consistent with the arachnoid cell phenotype.[97] The cells also stained negatively for myosin, S100, GFAP, CD31, SMA, and NeuN, indicating that they were not smooth muscle, glial, endothelial, fibroblast, or neuronal cells, respectively. As reported in other studies,[108],[109],[110] the cells appear similar to those in tissue fragments.

Collagen matrix preparation

Bovine Type I collagen was used to make porous sponges as per the protocol of Doillon et al.[108] A collagen dispersion (0.5% wt/volume) was made by slowly blending lyophilized insoluble collagen into a mixture with H₂O+ HCl solution (pH 3.0) at 4°C for 1 minute. After deaeration, the dispersion was poured into a pan, lyophilized at - 30°C, and dehydrothermally crosslinked in a vacuum oven at 110°C and 2.5 torrs for 5 days. Gamma irradiation (17,500 rads) was used to sterilize the sponges. The microstructure of the scaffold has two distinct regions that result from the freeze-drying process. The upper surface of the matrix has low porosity with cells seeded on this surface typically unable to penetrate deeply (Fig. 2.1). The bottom surface of the scaffold has high porosity with an average pore size of ~100 μm in diameter facilitating cell ingrowth. The scaffold was ~2–3mm thick and has a 3D architecture similar to the porous central core of an arachnoid granulation. This type of matrix has been used in previous investigations as a dermal replacement or a template for dermal regeneration,[109],[110],[111] and been used clinically for the treatment of dermal wounds.[112]

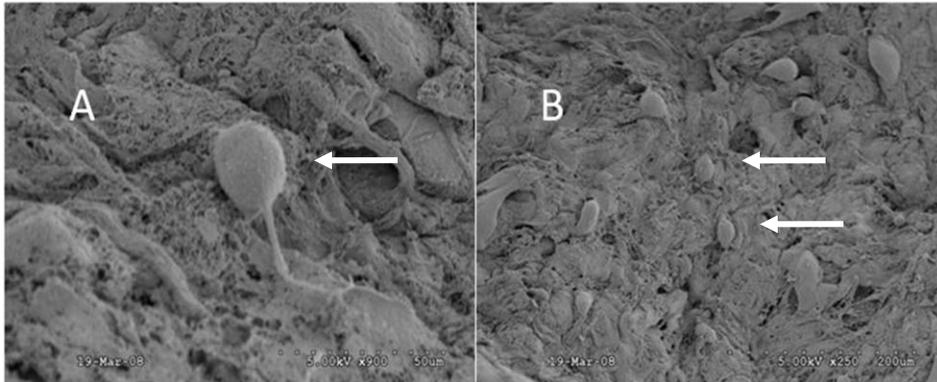


Figure 2.1: Arachnoid cells grown on microporous collagen
Arachnoid cells on a representative microporous side of bovine collagen scaffold by SEM. Panel A shows a cell (indicated with arrow) with a process that sends out smaller daughter processes. Panel B shows sparse growth of cells (two indicated with arrows) on substrate, which is similar to the natural state of the cells in an arachnoidal membrane.

Construct seeding and culture

Sterile sponges ~20mm in diameter were pre-equilibrated with culture media before seeding with rat cells. Approximately 50,000 arachnoid cells at passage 1–2 were used to seed the collagen sponges. Preliminary studies suggested that this seeding density was optimal for ensuring uniform and rapid population of the sponge. Constructs were cultured up to 21 days.

Histology and immunohistochemistry

Cells were permeabilized in 0.25% Triton X-100, blocked in 2% bovine serum albumin, and incubated with primary antibodies in PBS overnight at room temperature. After rinsing with PBS, cells were incubated with appropriate secondary antibody and counterstained with 4',6-diamidino-2-phenylindole (DAPI). Images were analyzed using a Biorad MRC-1024 single photon confocal microscope 1024 (Biorad Cell Science). For establishing arachnoid cell phenotype, cells

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were stained with cytokeratin 18 antibody (C-04, Abcam Inc.), vimentin (Prod #080552; Invitrogen), and desmoplakin I + II (Abcam, Inc.). Double labeling of vimentin and desmoplakin was done to help verify cell identification.

To verify purity of the arachnoid cell isolations, cells were also stained for the presence of potential contaminating cells: muscle, fibroblasts, endothelial cells, glial cells, and neuronal cells. Myosin (MA1-35718; Fisher Sci.) was used to identify muscle cells; S100 (13E2E2; BioGenex) and glial fibrillary acidic protein (GFAP, G-A-5; Cell Marque) were used to identify glial cells; CD31 (1A10; Cell Marque) was used to identify endothelial cells; smooth muscle actin (SMA asm-1; Novacastra) was used to identify fibroblasts; neuronal nuclei (NeuN, MAB377; Millipore) was used to identify neuronal cells. Staining levels for the cells were compared to positive controls (uterus, melanoma, brain, bladder cancer, uterus, and brain for myosin, S100, GFAP, CD31, SMA, and NeuN, respectively) or negative controls (brain for myosin, S100, CD31, and SMA, uterus for GFAP, and muscle for NeuN). The presence of gap junctions in cultures was determined by staining with connexin45 antibody (Prod #MAB3100; Millipore).

Scanning electron microscopy

Samples were fixed using 2.5% glutaraldehyde and 2.5% formaldehyde buffered to pH 7.4 with phosphate, followed by a serial dehydration in alcohol. Samples were dried using a critical point dryer (SPI # 13200-AB), sputter coated (SPI# 11429-AB), and imaged using a Hitachi HS 7S electron microscope.

Western immunoblotting

Confirmation of protein content to immunohistochemical staining was performed using Western blot. Positive controls were human A432 cell line (Abcam) and melanoma (Abcam) for desmoplakin and vimentin, respectively. Normoxia (a cell line donated by Dr. Roderick Barke, Minneapolis VA Medical Center: PC-12 [TCC # CRL-1721] adrenal gland from rat) was used as the negative control for both desmoplakin and vimentin. Approximately $1.0 \cdot 10^7$ cells were centrifuged at low speed for 5 min. Pellets were washed with PBS (prod # 17-512F; BioWhittaker) at room temperature and again centrifuged at low speed. PBS was carefully poured out and ice-cold RIPA buffer (product #89900; Pierce) with inhibitors (Sigma Protease

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Inhibitor Prod # P-8340; Sigma Aldrich and Aprotinin Prod # A6279; Sigma Aldrich) added and incubated on ice for 30 min. Proteins were denatured by boiling in water for 2–3 min and loaded into an 18 well Precast XT gel cassette (prod #345-0136; BioRad Hercules). Chemiluminescent Blue Ranger marker (prod # 26651; Pierce) and low range Rainbow marker (prod # RPN 755 E; Amersham) were used to reference molecular weights. Electrophoresis was performed using a Power Pac Universal (BioRad). Proteins in the gel were transferred to Hybond ECL nitrocellulose (prod # RPN 2020 D; Amersham) by sandwiching between thick Blot paper (prod # 1703967; Criterion BioRad) and run for 45 min at 10 volts using a Trans-blot SD (prod # 170-3940; BioRad). Nitrocellulose membranes were incubated with Startingblock (TBS) Blocking Buffer (prod # 3754; Pierce) for 60min on a rocker (Red Rocker Hoefer Scientific Instruments) at room temperature. The primary antibodies (Vimentin, Cytokeratin, and Desmoplakin) were diluted in TBST containing Startingblock at 1:1000 and were incubated overnight in the refrigerator on a rocker. On the following morning the nitrocellulose was rinsed twice with ~30 mL of TBST, incubated with Donkey Serum Block (prod # D9663; Sigma Aldrich) for 60 minutes, and washed twice with TBST for 5 min each. A 1:10,000 dilution of the secondary antibody (donkey anti-Rabbit IgG-Horseradish peroxidase conjugate; Amersham # NA934V) was then used to cover nitrocellulose for 60 minutes at room temperature. The sample was washed with TBST. Proteins were detected with SuperSignal West Pico (Pierce #34080). Autoradiography films (prod # RPN 2103; Amersham) were developed using a CP1000 (AGFA Mortsels).

DNA content assay, cell number, and morphometrics

DNA content was quantified with the DNeasy Blood and Tissue Kit (Qiagen Sciences).

Absorbance was measured, as per the manufacturer's instructions, at the 260nm wavelength.

Cell counts were performed using a hemocytometer (Hausser Scientific). cAMP was used to determine if it altered cell growth (1mg/mL of media).

Cell morphometrics was performed using ImageJ software from the NIH website. High-resolution digital images of the cells were obtained and maximal cell length and width measured. Width was determined perpendicular to the maximal length. Area was determined from image analysis of cell boundary traces. Process counting was done manually. Between 50 and 100 cells were used for process number analysis and morphometric measurements.

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Permeability

Transepithelial (arachnoid) electrical resistance. Transepithelial electrical resistance (TEER) was used as a measure of barrier function for cells grown on a monolayer.[113] Chopstick electrodes connected to an epithelial volt-ohmmeter resistance meter (World Precision Instruments, Inc.) were placed on the basal side and apical side of the membrane. Electrical resistance measurements were performed from day 5 to day 21 in culture and the resistance per unit area was determined by dividing values obtained by the surface area of the construct ($\sim 2 \text{ cm}^2$). The TEER value of a blank membrane (pore size $3.0 \mu\text{m}$; CoStar Transwell) was subtracted from the apparent TEER values of membranes with cells to obtain the effective TEER value. The membrane allows diffusion of small molecules such as ions.

Hydraulic permeability and dye transport. The permeability of indigo carmine (prod #55928, Sigma Aldrich) was quantified. The arachnoid cell construct was placed in a diffusion chamber (PermeGear Side-Bi-Side Cells) and maintained at 37°C . Each chamber was mixed using a magnetic stirring bar to minimize diffusion boundary layers at the interface of the construct. At 10 min intervals, 20 mL samples were taken from the receiver chamber and the concentration of the dye was determined using a Packard SpectraCount photometric microplate reader (measured at 520 nm)(Packard Instrument Co.).

The apparent permeability, P_{app} , of the cells to the dye can be estimated based on the following equation:

$$P_{app} = \frac{dC}{C_0 \times A \times dt} \quad (1)$$

where dC/dt is the slope of the change in concentration in the chamber as a function of time obtained directly from measurements, C_0 is the initial concentration of dye on the inlet side of the diffusion chamber, and A is the area through which the dye permeates.[114]

The actual permeability (P) of the cell monolayer to dye is derived after correcting for the resistance to dye permeation from the membrane

$$\frac{1}{P} = \frac{1}{P_{app}} - \frac{1}{P_m} \quad (2)$$

where P_m is the permeability across the membrane without cells.

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To measure hydraulic conductivity, the arachnoid construct (1 cm diameter) at day 10 in culture was placed in a horizontal Ussing chamber. A pressure gradient (3.67mmHg) was applied on the upstream chamber and water flow through the chamber was measured (final volume–initial volume). These measurements were used to estimate the hydraulic conductivity, L_p , of the construct:

$$L_{p, scaffold} = \frac{Q_{scaffold+filter}}{\Delta PA \left(1 - \frac{Q_{scaffold+filter}}{Q_{filter}} \right)} \quad (3)$$

where Q is the flow of water, DP is the pressure drop across the membrane (3.67 mmHg), A is the area across which the water flows.[35]

Statistics

Analysis of variance was used to analyze cell proliferation (DNA content with time) and changes in cell morphology determined using image analysis. Changes in hydraulic or dye permeability were analyzed using a paired t test. Analysis of variances and t tests were performed using SPSS software.

Results

Arachnoid cell isolation

Arachnoid cells isolated from brain tissue (Fig. 2.2 for cells on brain stem) contained cytokeratin both in cultures grown on 2D culture wells (Fig. 2.3A) and in 3D collagen sponges (Fig. 2.3B), as confirmed by western blotting.

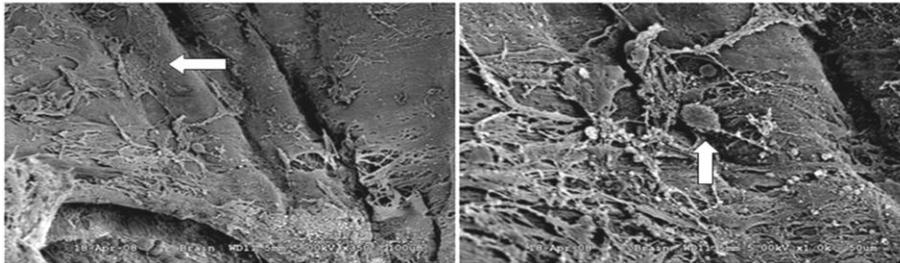


Figure 2.2: Scanning electron microscopy of native rat pia-arachnoid tissue. Cell process (A) and Arachnoid cell (B) are denoted by arrows.

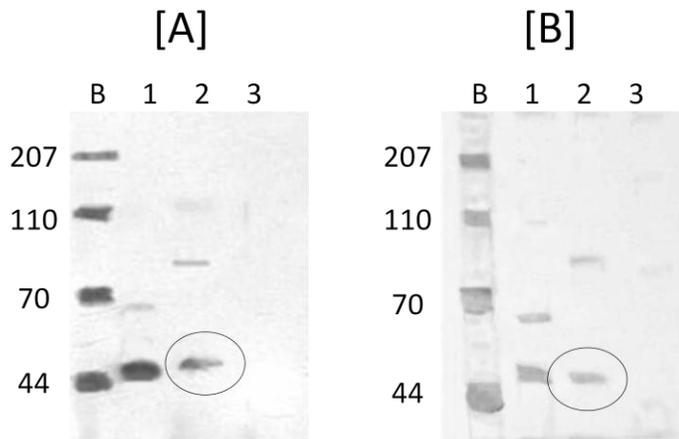


Figure 2.3. Western blot for cytokeratin isolated from rat arachnoid cells on tissue culture surface (A) and collagen matrix (B) protein molecular mass marker (Blue Ranger; Pierce) with bands at 44 kDa to 207 is lane B. Lane 1 is positive control (HeLa cells). Lane 2 is

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rat arachnoid cells showing positive cytokeratin band at 45 kDa (circle). Lane 3 is negative control (adrenal).

Expression levels of desmoplakin and vimentin for the cultures were also confirmed through western blots (Fig. 2.4), and demonstrated colocalization of desmoplakin with vimentin consistent with the arachnoid phenotype.[33] To differentiate arachnoid cells from other cell types found in the intracranial cavity, the cells were stained for the presence of myosin, S100, GFAP, SMA, and CD31. The cells stained negatively for these markers, indicating that the cells isolated were not endothelia, neurons, glia, myocytes, or fibroblasts.

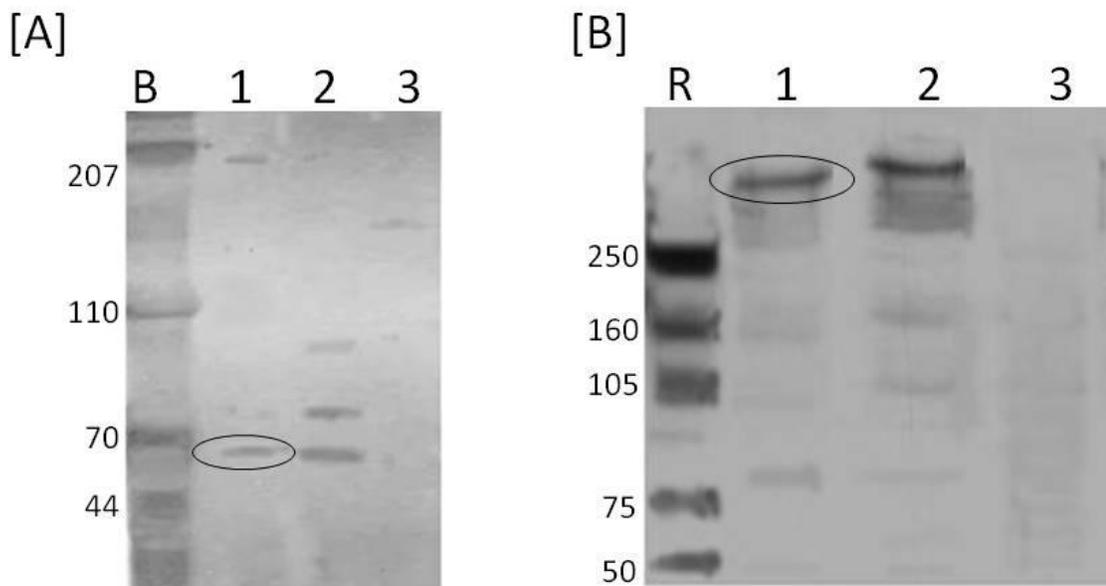


Figure 2.4: Western blotting of cells from 2D culture plates for identifying markers, vimentin [A] and desmoplakin [B]. The circled bands show vimentin [A] positivity at 57 kDa and desmoplakin [B] positivity at 331 kDa in arachnoid cells. Lane R, mass marker (Rainbow), shows marks at 50 kDa and 250 kDa. Lane B (Blue Ranger) shows mark at 44 and 70 kDa. Lanes 2 (HeLa cells) are positive controls. Lanes 3 (adrenal) are negative controls.

Cell culture on tissue culture plastic

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Arachnoid cells on 2D culture plates were predominantly bipolar (Fig. 2.5A), and stained positively for vimentin (Fig. 2.5B) and cytokeratin (Fig. 2.5C). Hematoxylin and eosin staining demonstrated the presence of large nuclei and long spindly processes in greater detail than the immunostaining (Fig. 2.5D).

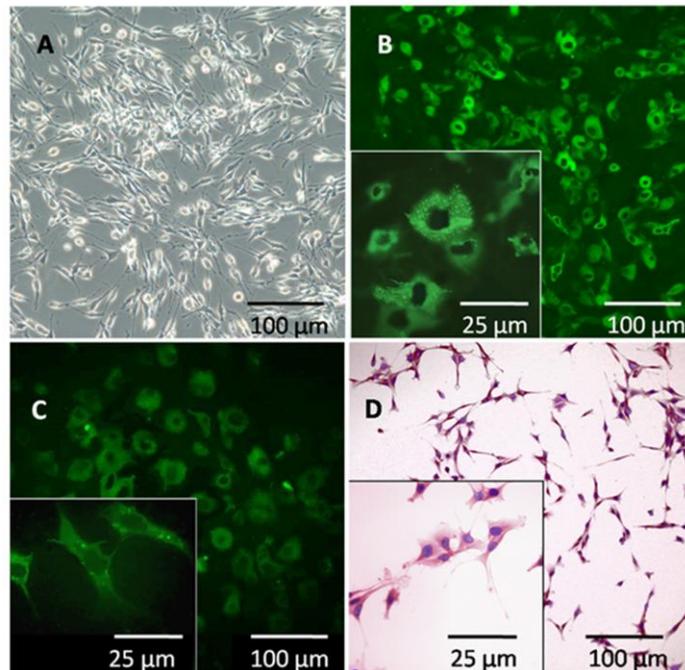


Figure 2.5. Morphology and staining patterns of rat arachnoid cells on tissue culture plastic: (A) Phase-contrast light micrograph of arachnoid cells after 3 days in culture. (B) Fluorescent micrograph of cultures stained for vimentin. (C) Fluorescent micrograph of cultures stained for cytokeratin. (D) Hematoxylin and eosin staining of arachnoid cells 3 days in culture.

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The cells proliferated with a doubling time of ~ 3 days (Fig. 2.6A) and cell doubling times were consistent (as determined using cell counts and DNA content) (Fig 2.6B).

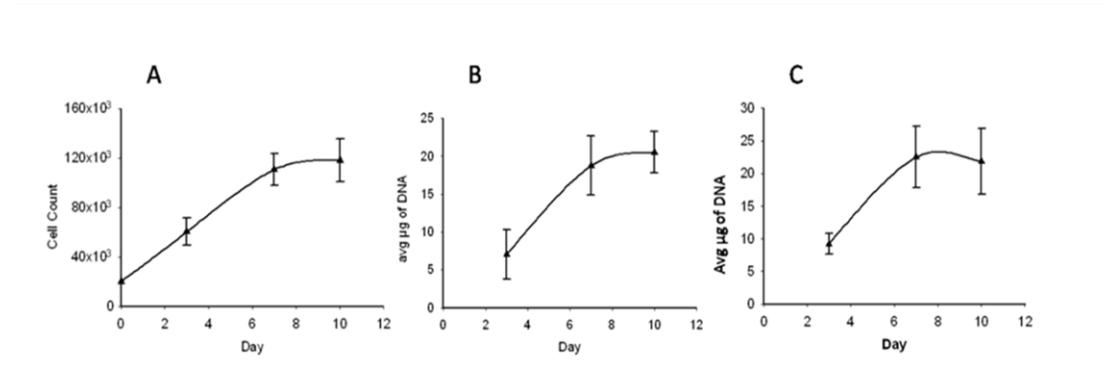


Figure 2.6: Growth curve for arachnoid cells cultured on tissue culture plastic and collagen scaffold: (A) Cell counts as a function of time in culture for arachnoid cells cultured on culture wells; (B) DNA content of arachnoid cells grown on culture wells as a function of time in culture; and (C) DNA content of arachnoid cells grown in a collagen matrix as a function of time in culture. Error bars indicate standard error (n=4).

The addition of cAMP to the culture medium did not alter the growth rate of the cells ($p = 0.14$ by paired t test). Cultures were stained for the presence of gap junction proteins (connexin) at days 5, 10, and 15. Initially, areas of punctuate fluorescence indicative of gap junction formation were seen over the cell layer. By ~ 3 weeks, connexin staining exhibits two different staining patterns (1) punctate (which was more intense) and (2) diffuse (less intense) (Fig. 2.7).

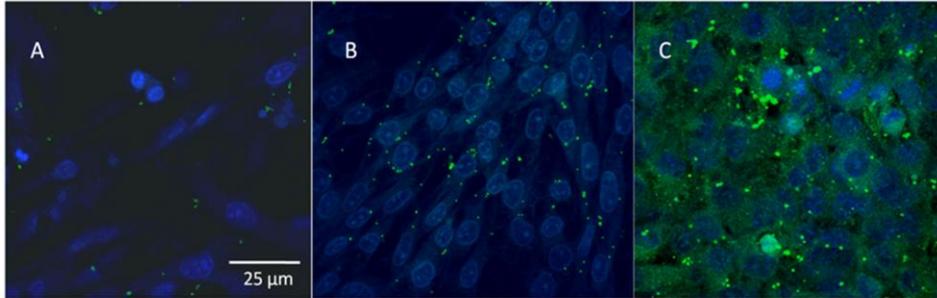


Figure 2.7: Connexin staining changing over time

Arachnoid cells increasingly expressed connexin as culture matures. At day 5 (panel A), punctate immunofluorescence is seen as is expected from junctional proteins. By day 10 (panel B), the spots are more numerous and gravitates toward the edges of the cells. By day 15 (panel C), expression becomes more fine and diffuse over the cells similarly to other published results.

Physiological behavior of arachnoid cell monolayers

In the native tissue, the arachnoid granulation forms a functional barrier to the flow of CSF. To quantify the barrier function of arachnoid cell monolayers, we measured (1) TEER[115] and (2) permeability to indigo carmine.[116] TEER values increased with time in culture and achieved the maximum value of $160 \Omega \cdot \text{cm}^2$ after 15 days in culture and no further increases were observed. Permeability of cell monolayers to indigo carmine was also quantified. The dye was introduced into one side of the diffusion chamber and the concentration of dye in the other chamber was monitored as a function of time (Fig. 2.8). These data were analyzed using the equation above (Equation 2) to obtain an estimate for the permeability of the cell monolayer. The dye permeability of the arachnoid cells was $6.7 \cdot 10^{-6} \pm 1.1 \cdot 10^{-6} \text{ cm/s}$.

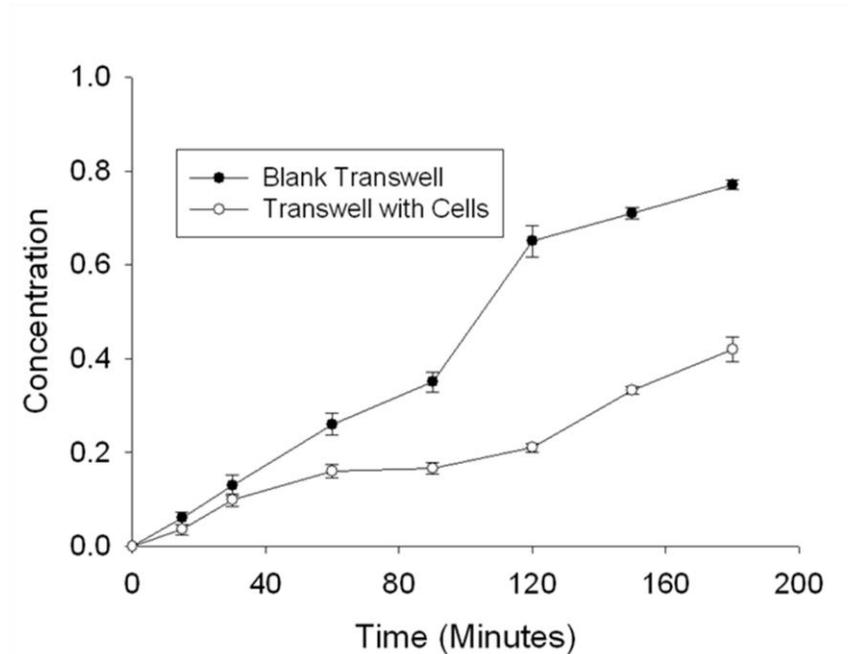


Figure 2.8: Permeation of Indigo Carmine through a monolayer of arachnoid cells: Transwell without cells (black circles, n=6) and a Transwell cultured with monolayer of arachnoid cells (open circles, n=6).

Arachnoid culture in a collagen scaffold

The arachnoid cells attached to the collagen scaffold readily (Fig. 2.9). Preliminary seeding studies were performed to determine the minimum seeding density to achieve population of the matrix. Seeding densities of 10,000, 20,000, and 100,000 cells per well or $\sim 5,000$ to $50,000$ cells/cm² were tried. A seeding density of $50,000$ cells/cm² resulted in the most rapid repopulation of the matrix. Increasing seeding levels to higher values did not increase the rate at which the matrix was repopulated. DNA content in the matrix reached steady state within 7 days (Fig. 2.6C). Confocal microscopy was used to determine the spatial distribution of cells throughout the matrix (Fig. 2.9A, B) and the phenotype of the cells (e.g., expressing desmoplakin and vimentin as shown in Western blotting) (Fig. 2.9C, D). Cells populated the collagen sponge

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uniformly (see supplementary 3D video) and electron microscopy revealed that cell morphology was consistent with that observed in native tissue (Fig. 2.9B). Even though cells penetrated well into the scaffold, cell distribution remained sparse throughout the scaffold, which is consistent with the cell distribution observed in the arachnoid core.[40]

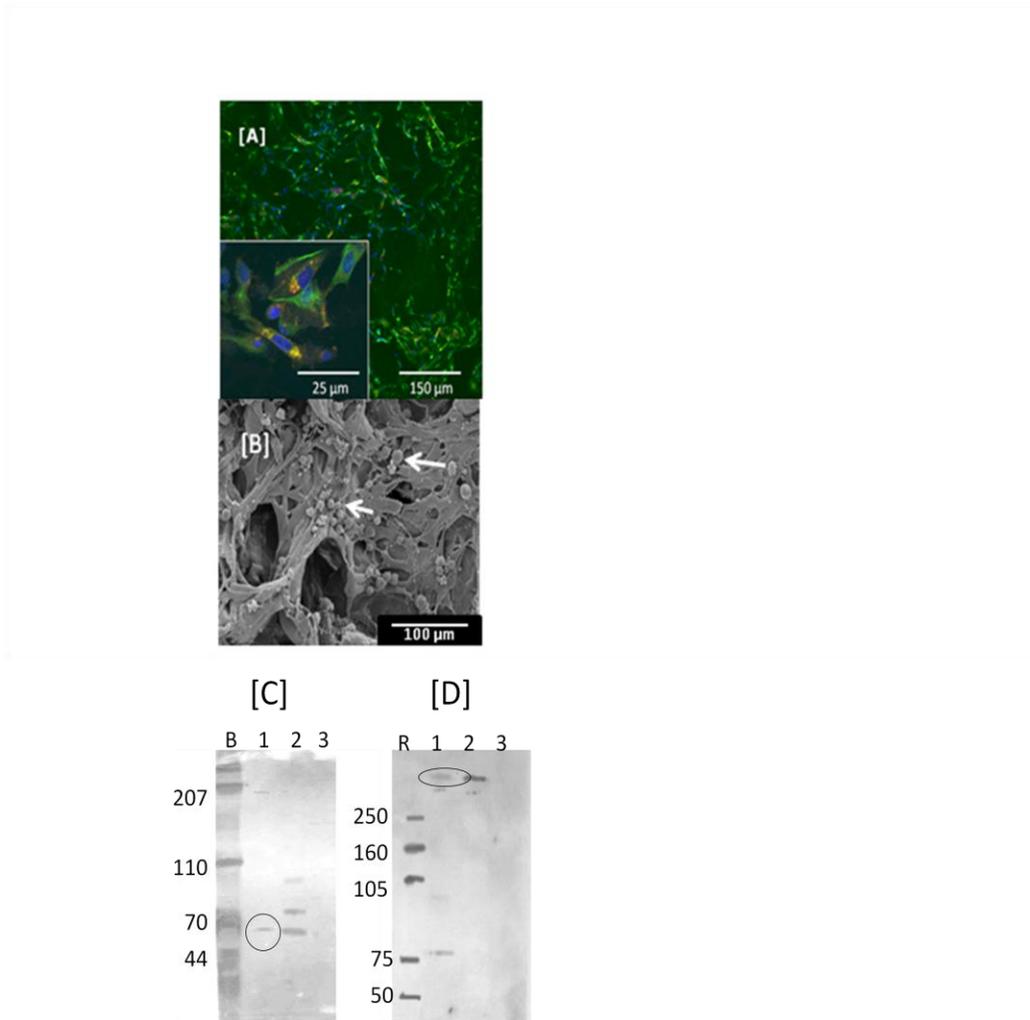


Figure 2.9: Arachnoid cells grown on porous collagen scaffolds with pore size of approximately 100 µm: (A) Scanning confocal micrograph of arachnoid cells cultured on a collagen matrix stained with desmoplakin (R-Phycoerythrin; emission 575 nm) and vimentin (Fluorescein; wavelength emission 528 nm). DAPI was used for nuclear staining. Yellow

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represents additive summation of the primary colors red and green indicating co-localization

(B) Scanning electron micrograph (SEM) of arachnoid cells cultured on a collagen matrix, arrows indicate individual cells (C) Protein expression for vimentin in scaffold (57 kDA, Lane 1, circled). With 50 kDA mass marker is Rainbow in Lane R. Lanes 2 and 3 are positive (HeLa) and negative controls (adrenal) respectively. (D) Protein expression for desmoplakin (331 kDA, Lane 1, circled). Protein mass marker (Blue Ranger) is lane B, with lanes 2 and 3, positive (HeLa) and negative (adrenal) controls respectively.

Morphometric analysis of cells grown on 2D and 3D surfaces

Arachnoid cell body geometry on 2D cultures was determined quantitatively at 6, 12, and 18 days after seeding (Fig. 2.10). Specifically, length, width, and area of the cells were quantified. The cell area did not change with time in culture, but cells became significantly shorter over time (day 6–18) ($p = 0.02$). The number of cell processes did not differ over that same period and the variation of length appears to occur both with cells of low and high passages (passage > 8). Likewise, the process formation was not different between the 2D cultures compared to the collagen scaffold preparations (Fig. 2.11 compared to Fig. 2.9B). The morphology of the cells cultured in the construct was also determined using scanning electron microscopy. Most cells exhibited extensive bipolar process formation, which appeared to penetrate into the scaffold (Fig. 2.9B). Arachnoid cells of similar shape were also found on the apical (nonseeded microporous) side (Fig. 1.1). The number of processes was not significantly different between cells grown on 2D culture plates compared to that of cells grown in a 3D collagen sponge (Table 2.1).

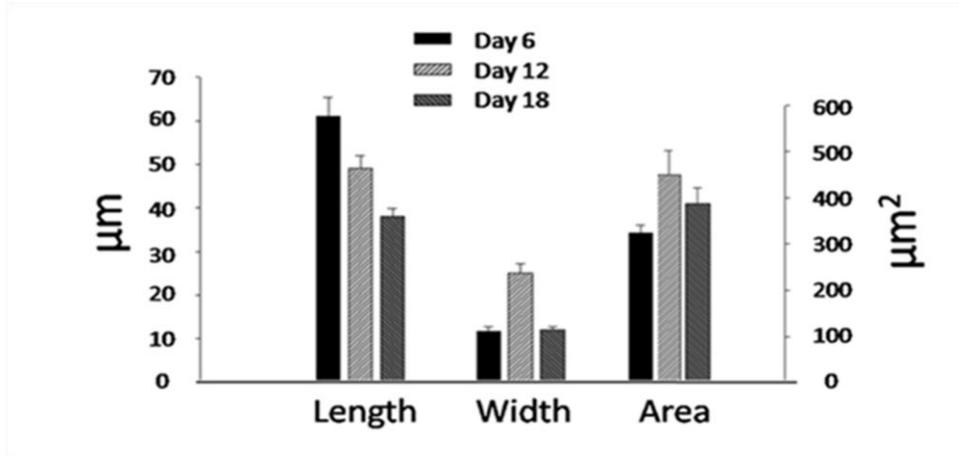


Figure 2.10: Morphometric analysis of arachnoid cells. Length, width and area of arachnoid cells grown on tissue culture. Error bars indicate standard error.

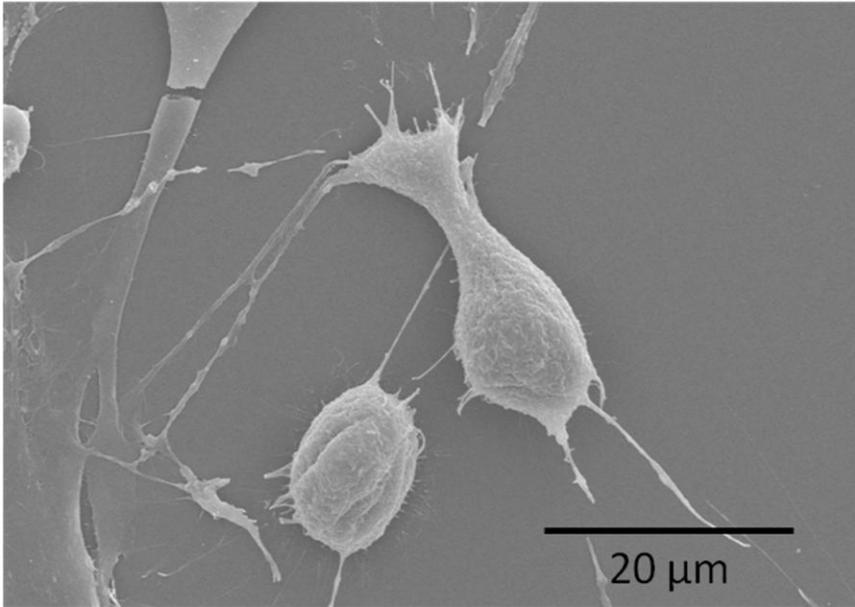


Figure 2.11: Scanning electron microscopy of arachnoid cell on culture plate. Processes may be seen emanating from the cells. They appear similar to the cells on a collagen scaffold.

Table 2.1: Average number of processes per cell (n =50) on 2d culture plates compared to 3d collagen sponges on day 6, 12, and 18. Standard error of the mean is given in parentheses.

	Day 6	Day 12	Day 18
2d culture plate	2.15 (0.081)	2.25 (0.101)	2.03 (0.084)
3d collagen sponge	2.2 (0.117)	2.35 (0.121)	2.14 (0.102)

Physiological behavior of arachnoid construct

An arachnoid construct after 10 days in culture was placed on a Transwell insert and inserted in an Ussing chamber. The flow of water through the construct was measured for a constant pressure difference (3.67 mmHg). The hydraulic permeability for the construct was 6.39 ± 1.53 mL/min/mmHg/cm². The hydraulic permeability of the collagen matrix alone was 7.07 ± 1.56 mL/min/mmHg/cm². The difference between the two permeabilities was not statistically significant (two-tailed independent t test, $p = 0.256$).

Discussion

Cell culture on tissue culture plastic

Cells isolated from the tissue exhibited arachnoid cell phenotype: cytokeratin positivity, co-expression of desmoplakin and vimentin, and formation of gap junctions when cultures become confluent. We have also established that the arachnoid cultures that were isolated were not contaminated with other cells present in the native tissue (fibroblast, muscle, endothelial, glial, and neuronal cells). Expression of vimentin and desmoplakin found in the cultures that were

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isolated in this investigation exhibited similar phenotype to arachnoid cells isolated from human granulation,[34] spinal,[32] fetal[115] tissue, and other locations in the brain.[98]

A unique aspect of native arachnoid cells is their ability to form the CSF–blood barrier. Previous investigations have demonstrated that human granulations exhibit tight junction formation, which has also been associated with barrier formation.[109] Zonula Occludens-1 (a component of tight junctions) and E-cadherin (a calcium dependent cell adhesion molecule) have been found in previous studies of arachnoid cell culture.[34] Also, desmosomes, which are made up of multiple proteins, including desmoplakin, have been observed in arachnoid cultures using transmission electron microscopy.[117] The role of calcium is uncertain. In vivo manifestations of calcium in granulations typically are in isolated concretions that are not within the pathways of water movement. In this study, we have shown that gap junctions (as determined by connexin staining) develop in culture and become more numerous with time in culture.

The barrier capability of cell monolayers cultured in vitro has been studied using a variety of methods, including TEER. TEER values for monolayer cultures of Madin–Darby Canine Kidney Cells (MDCK II) and human colonic adenocarcinoma cells (caco-2) range between 100 and 500 $\Omega\cdot\text{cm}^2$, respectively.[73] In this investigation, TEER values of 160 $\Omega\cdot\text{cm}^2$ are well within the range of values measured for other models of blood–brain barrier. It is noteworthy that the ECV304 and HCMEC/D3 cell lines have been used as an in vitro model of the blood-brain-barrier[118], and TEER values for these cells have been measured at $\sim 110 \Omega\cdot\text{cm}^2$. With TEER of 160 $\Omega\cdot\text{cm}^2$, we demonstrate the first CSF–blood barrier formation capability in an in vitro model. Transport function of the arachnoid monolayer also has been quantified via the permeation of dyes. By way of comparison, the permeability of Lucifer Yellow for caco-2 cells was $2.5\text{--}5.0 \cdot 10^{-6} \text{ cm/s}$ and MDR-MDCK cells was $6.0\text{--}8.0 \cdot 10^{-6} \text{ cm/s}$. [114] A recent study demonstrated permeability of Lucifer Yellow for human arachnoid cells in cell culture inserts to be $7\text{--}14 \cdot 10^{-6} \text{ cm/s}$. [36] The permeability of indigo carmine in arachnoidal cells measured in this investigation was well within the range of these previously measured permeabilities ($6.7 \cdot 10^{-6} \text{ cm/s}$).

Arachnoid culture in a collagen scaffold

Arachnoid cells that were seeded into the matrix rapidly repopulated the matrix (~ 7 days). Cells grown on a collagen sponge (diameter of 16mm) contained slightly more DNA content on

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average than cells grown on tissue culture plastic (36mm in diameter) after the same time period (7 days). This suggests that cell densities from collagen sponges are growing at a rate similar to or slightly higher than cells grown on tissue culture plastic. Overall, the density of cells on the surface of collagen sponges (viewed by scanning electron microscopy) appear to be consistent with the sparse density of arachnoid cells in the native tissue.[44] As with arachnoid cells cultured on tissue culture plastic, arachnoid cells cultured in the collagen matrix exhibited the expected phenotype (expression of desmoplakin and vimentin). Cells cultured in the construct were principally bipolar. This cell shape is consistent with that observed in certain native tissues,[119] and there was little difference in morphometry between cells cultured on tissue culture plastic and in the collagen matrix. The hydraulic permeability measured in this investigation ($\sim 6 \cdot 10^{-6}$ cm/s) was slightly higher than that measured in another study with human arachnoid cells ($\sim 3 \cdot 10^{-6}$ cm/s).[36] It is currently unclear as to the reason for the decrease in hydraulic permeability measured in this investigation although they are within the same range. Because the PET is a nonwoven fibrous mat, a direct comparison is difficult.[104] PET is a synthetic matrix that replicates neither the biological signaling of collagen nor the spongy architecture of the native arachnoid granulation. In contrast to previous studies, we were able to recapitulate the two distinct layers in the arachnoid tissue, the core (collagen sponge studies) and the cap (monolayer studies), and demonstrated function of the cells in these two contexts. The use of a biocompatible and degradable material such as collagen is also important for any potential future uses (or implantation). Minute contaminants on nonbiologic substances in the brain are extremely difficult to treat; therefore, infections of artificial ventriculoperitoneal shunts almost always require removal. This complication is one of the most common complications of shunting.[45] Therefore, the utilization of collagen would be an important step in the creation of a bioartificial construct as a means for diverting CSF. The density of cells in the construct is much less than that in cell monolayers but mirrors more closely the density of arachnoid cells in the core region of the native granulation. Additional studies are currently being pursued to stratify cell density in the construct to mirror that in the native tissue. In summary, the results of this study demonstrate that arachnoid cells can be isolated from native rat brain tissue and successfully cultured ex vivo in monolayers and collagen scaffolds. The cells express arachnoid cell phenotype and demonstrate aspects of

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normal arachnoid granulation function (barrier to the flow of water and larger molecules). This in vitro model of the arachnoid granulation has the potential to help us both understand the causes/development of hydrocephalus and develop tissue engineered alternatives to conventional methods of treatment.

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Supplement Movie: Three D movie demonstrating cell penetration into scaffold: Three dimensional view of the collagen scaffold populated by the arachnoid cells. The movie rotates the scaffold on edge so that penetration by the cell is visualized. Scaffold thickness is approximately 2mm. Available at: www.liebertonline.com/tea.

Chapter 3: Immortalization and Functional Characterization of Rat

Arachnoid Cell lines

Creation of a stable cellular substrate for the study of arachnoidal transport and tissue engineering

The availability of primary arachnoid cells is limited. Harvesting the tissue from rodents is difficult and requires multiple animals for the assembly of sufficient cells for physiologic work. The cells are fickle and older animals not only do not grow well, but also vary in its transport abilities. This therefore serves as the impetus for the development of an immortalized cell line of rat arachnoid. One previous attempt, while able to maintain cells for a longer period than primary cells ultimately failed when multiple passages were carried out. We therefore set out to on the same task, but applied newer techniques of immortalization. To this aim, we developed two lines of stable cell lines, one using a tried technique of LgTAg adenovirus transduction, the second using a double immortalization technique of LgTAg plus human TERT transduction. These two cell lines function identically. This paper describes these cell lines and gives preliminary physiologic data particularly of transport.

The work is carried out by Christopher Janson, Liudmila Romanova, Eric Hansen, and Cornelius Lam. The paper is written by Christopher Janson, Liudmila Romanova, and Cornelius Lam.

Abbreviations: CSF, cerebrospinal fluid; DT, double-transduced; FBS, fetal bovine serum; hTERT, human telomerase; LTA_g, large T antigen; PBS, phosphate buffered saline; rTERT, rat telomerase; SEM, scanning electron microscopy; ST, single-transduced; TEER, transmembrane electrical epithelial resistance; TPG, total product generated; TRAP, telomerase repeat amplification protocol.

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Introduction

The arachnoid mater, which along with pia mater forms the leptomeninges, exists between the CNS and the dura mater. Embryologically it is derived from neuroectoderm and extends from the most caudal extent of the filum terminale to the external surface of the cerebrum. Because of the different local environments where arachnoid cells may exist, such as at the nerve root sleeve or within the dural venous sinus, cellular phenotypes are variable, though typically consist of elongated, spindle-shaped epithelial cells. Similar to choroid plexus, arachnoid cells maintain apical-basal polarity and form tight junctions which create a barrier to solute and water flow (i.e. CSF-blood barrier).

Arachnoid cells comprise the core of the arachnoid granulation, a major site of egress for cerebrospinal fluid (CSF) to the venous system, which is affected in communicating hydrocephalus and other brain disorders involving abnormal flow of CSF. The production and bulk resorption of CSF has been studied *in vivo* with mammalian models, but molecular mechanisms involved in solute and water transport at the level of the arachnoid villi remain poorly understood. Use of primary arachnoid cells [120],[34],[104] for *in vitro* studies has numerous practical limitations due to their low proliferative rate and early senescence, which typically occurs after 4–8 passages. Our preliminary work with rat primary cultures indicated that arachnoid cells did not approach confluence when seeded into a three-dimensional collagen framework, and two-dimensional systems were likewise constrained by poor growth properties of source material after very early passage. Primary cultures required repeated collection of tissue due to rapid senescence and underscored the need for generation of stable cell lines. The purpose of this study, therefore, was to generate stable cell lines derived from normal mammalian arachnoid villi or dissociated arachnoid cells, similar to native cells in their morphology and physiology, to be used in studies of CSF flow.

In general, primary explanted cells in culture grow for only a limited number of population doublings until they reach the first replicative barrier, known as M1 or senescence, which is defined as irreversible proliferative arrest in the presence of ongoing metabolic activity [121]. Human cells have a further barrier, which is known as M2 or crisis, which is defined as widespread cell death despite ongoing cell division [122]. M1 arrest is primarily related to

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expression of tumor suppressor genes such as p53 and Rb, while M2 arrest is primarily related to telomere shortening with repeated cell divisions [123]. This progressive telomeric shortening with repeated DNA replication cycles may be partially offset by telomerase reverse transcriptase, which maintains telomere length in germline and stem cells. Immortalized cells are those which have bypassed both M1 and M2.

In human cells, addition of viral oncogenes such as SV40 large T-antigen (LTA_g) or adenovirus E1A typically leads to extension of life without true immortalization. The mechanism for LTA_g effects on the cell cycle is primarily through binding to and inactivating p53 and Rb tumor suppressors [124]. In mouse or hamster cells, which have a limited life span of 20–30 generations in culture, LTA_g transduction alone is usually sufficient for immortalization with efficiency approaching 100% [125]. The additional step of telomerase activation is required for human cell immortalization, and ectopic expression of human telomerase (hTERT) in human cells permits telomerase-negative cells transformed with LTA_g to bypass senescence [126]. In addition to species-specific constraints, cells of different lineages or tissues of origin may have slightly different requirements for immortalization [127]. For example, single transduction with hTERT in human fibroblasts, endothelial cells, and mesothelial cells may be sufficient to bypass senescence [128] while other cells such as keratinocytes or mammary epithelial cells may require co-expression of other factors [129].

There is a prior report of an “immortal” cell line created from normal human arachnoid cells with LTA_g transduction [97], but this cell line is no longer available and actually was a senescent cell line at P50 which changed its immunohistochemical and functional characteristics over time, gradually losing cytokeratin markers after P30. Several other groups have reported transformation of human meningioma cells and formation of cell lines either using hTERT alone [130] or hTERT with SV40 LTA_g [131]. In one cell line derived from low-grade human meningioma, expression of hTERT alone allowed passaging through P20 but the cells eventually became senescent and required treatment with other viral oncogenes to become immortal [132], which serves to emphasize cell-type specific mechanisms of senescence that depend on a number of complex factors working in concert to overcome M1 and M2.

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A major advantage of rat arachnoid cells is that they represent a readily available and homogenous source compared to human material from different donors, and may be transplanted into various rat models of inherited or induced hydrocephalus [133],[134]. Because the replicative potential of rat arachnoid cells was largely unknown and the cells appeared to become senescent after a very limited number of passages, we began by transforming cells with SV40 LTA_g and then double-transformed a subset of cells with SV40 LTA_g and hTERT. A variety of immortalization strategies have been described in the literature, including use of adenoviral E1a, human papilloma virus16 E6/7, and other physical or chemical approaches [135], but the most widely used and reliable methods utilize SV40 LTA_g and/or telomerase.

While in human cells telomerase activity is highly regulated and repressed, mouse and hamster cells promiscuously express telomerase in most somatic cells, which (in addition to longer telomere length of 20–100 kb compared to 0.5–15 kb in human cells) may contribute to their tendency to be readily immortalized. Interestingly, mouse telomerase (mTERT) is expressed in the adult mouse testis and liver but is not detected in brain [136] outside of putative stem cells. Rat telomerase (rTERT) was recently cloned [137] but constructs are not readily available and considerably less is known about its activity, though it appears to be upregulated in adult rat testis, liver and brain compared to other tissues and has activity similar to hTERT and mTERT. Telomerase expression in normal human arachnoid cells remains unknown, but is often found in meningioma tissue and directly correlates with tumor malignancy [138].

There is known to be crosstalk between telomerase and various cell cycle pathways; for example, hTERT inactivates the tumor suppressors p16 and Rb [139] and is itself suppressed by Rb and p21 but stimulated by c-myc, which suggests that inhibition of Rb through SV40 LTA_g transduction could have indirect effects on telomerase [140]. In the past, rat astrocytes [141] or neurons [142],[143],[144] have been immortalized with a single-step SV40 LTA_g strategy, which is predicted to upregulate endogenous telomerase, though this had never been directly tested. Rat cells are not as commonly used or as well defined as mouse cells, and in the case of arachnoid cells, it was unknown if cells would show synergistic growth and viability with additional telomerase.

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In summary, we expected that LTA_g would suffice for immortalization, but given the limited growth of primary cells, it was predicted that transduction with hTERT would confer benefits in doubling time and long-term viability. Surprisingly, we found that significant upregulation of telomerase in double-transduced (DT) cells did not augment the growth profile or otherwise alter the phenotype of cells at over 160 passages, compared to single-transduced (ST) cells. Thus, minimal SV40 immortalization appears sufficient in rat arachnoid cells. We also demonstrated that, specifically within arachnoid cells, rat telomerase is active at baseline and addition of LTA_g did upregulate native rat telomerase. We observed a stable immortalized phenotype in both ST and DT cell lines, with superior functional properties for physiological studies compared to primary cells.

Experimental procedures

Primary culture of rat arachnoid cells

Arachnoid cells were harvested from 21 to 23 day old female Sprague–Dawley rats. The animals were euthanized with CO₂ according to an approved VA Medical Center animal protocol. Carcasses were thoroughly cleaned with 70% ethanol. The cranium and cervical spine were exposed and the brain and upper spinal cord was removed en bloc. The leptomeninges were removed by gentle dissection from the brainstem and finely minced with a #15 scalpel, then placed in Dulbecco's modified Eagle's medium (DMEM, Invitrogen) with 10% heat-inactivated fetal bovine serum (FBS) containing 1% penicillin/streptomycin (Gibco) in a six-well poly-L-lysine coated plate (BD Biosciences) in a humidified incubator at 37 °C with 5% CO₂ atmosphere. The next day culture media was replaced without disturbing the cells. After the cells became adherent, they were split at a 1:2 to 1:6 ratio every 7 days. At passage 3 or 4, arachnoid cells were replated into a Biocoat six-well poly-D-lysine coated plate (BD Biosciences). Viral transduction was performed when the cells reached 60–80% confluence.

Production of retrovirus containing SV40 LgTA_g and hTERT

Retroviral constructs pBABE-neo-hTERT and pBABE-puro-SV40LT, containing hTERT or SV40 LTA_g along with the G418 or puromycin resistance genes, were manufactured by Dr. Robert Weinberg, MIT-Whitehead Institute, and obtained through a nonprofit plasmid repository (Addgene). The plasmids were expanded from transformed bacterial cultures, column purified,

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and verified for fidelity with restriction digests. Plasmids were then used to transfect EcoPack2 cells (Clontech), which are 293HEK ecotropic feeder cells containing retroviral packaging genes. EcoPack2 cells were seeded 12–18 h prior to use at 5×10^5 cells/25 cm² flask. Then 5 µg of pBABE-puro-SV40LT was combined with Fugene reagent (Roche) and OptiMem (Invitrogen) serum-free media in 250 µl total reaction volume with 3:1 ratio of Fugene:DNA. This was incubated for 30 min and added to each flask of 293HEK ecotropic feeder cells, with 3 ml of serum-containing media per flask. After exactly 48 h, the retroviral supernatant was collected, pooled from each flask into a 50 ml tube, and clarified with Millipore PVDF 0.45 µm Steri-Flip vacuum membrane to remove cellular debris. From six flasks, 18 ml total supernatant was collected. Quantitative RT-PCR was then used to obtain viral particle titers, using primers from the Retro-X qRT-PCR titration kit (Clontech), and RNA genomic titers were confirmed to be $>2 \times 10^9$ /ml.

Retroviral transduction of arachnoid cells

Clarified viral supernatant containing pBABE-puro-SV40LT was applied to the arachnoid cell primary culture. Target cells were initially at a density of 4×10^4 cells/well of a six-well plate. Media was aspirated and 3 ml virus-containing media was added per well. Polybrene (Millipore) was added to a final concentration of 4 µg/ml. After 12–18 h of incubation, virus-containing media was aspirated and replaced with fresh media, to avoid polybrene toxicity and possible adverse effects from conditioned media. Cells transduced with pBABE-puro-SV40LT were selected over 14 days with puromycin (Sigma). Selection was started with 0.5 µg/ml puromycin, then increased to 0.75 µg/ml. A subset of these cells was stored and additional cells were then double-transduced with the pBABE-neo-hTERT construct and selected with G-418 (Calbiochem) at 200–400 µg/ml. The single- and double-transduced cells were expanded in 75 cm² flasks and aliquots were frozen in liquid nitrogen in Recovery™ cryopreservation media (Invitrogen) for future use. Banked cells were verified free of mycoplasma contamination using MycoAlert assay (Lonza).

Immunostaining

Cells were grown on four-well poly-D-lysine culture slides (BD Biocoat) and fixed with 4% formaldehyde in phosphate buffered saline (PBS). The cells were permeabilized with 0.5% Triton X-100 in PBS for 5–7 min and washed 3X with a washing solution containing 10% FBS and 0.2%

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Tween-20 in PBS before application of primary antibodies. Double-staining was carried out sequentially as needed with species-specific primary antibodies. In general, cells were incubated with primary antibodies for 1 h, washed with the washing solution and incubated with secondary antibodies for 1 h. Finally, cells were washed with washing solution and nuclei were stained with Hoechst dye (Sigma) for 15 min. Slides were air-dried and water-soluble fluorescence mounting solution (Dako) and cover slips were applied. Fluorescence images were captured with a Nikon Eclipse E600 microscope with Diagnostic Instruments Spot Insight CCD camera. Images were post-processed with Adobe Photoshop CS3. The following antibodies and dilutions were used for immunostaining: rabbit monoclonal anti-hTERT (Abcam, Cat. #32020) at 1:20, mouse monoclonal anti-SV40 LTA_g (Abcam, Cat. #16879) at 1:50, rabbit antivimentin antisera (Abcam, Cat. #8545) at 1:1, rabbit polyclonal anti-cytokeratin (Dako, Cat. #Z0622) at 1:100, mouse monoclonal anti-cytokeratin18 (Abcam, Cat. #668) at 1:20, mouse monoclonal anti-desmoplakin (Abcam, Cat. #16434) at 1:10. The following secondary antibodies were used, all at 1:500 dilution: Alexa Fluor 488-conjugated anti-rabbit or anti-mouse IgG (Invitrogen), Alexa Fluor 555-conjugated anti-rabbit.

Western blotting

Cell extracts were prepared from 5×10^5 cells as described previously [145]. Extracted proteins were resolved in a 10% or 12% SDS PAGE gel and transferred onto immobilon-P membrane (Millipore) for immuno-detection. The membrane was treated with blocking solution containing 5% skim milk and 0.2% Tween-20 in PBS for 1 h. The primary antibodies were used as cited above, at concentrations according to the manufacturer. The incubation time with primary or secondary antibody was 1 h. Signal was detected by using SuperSignal West Dura (Pierce Biotechnology) as a substrate for peroxidase. The primary antibodies were used as cited above, at concentrations according to the manufacturer. GAPDH was used for loading controls, in addition to cell counting. The secondary antibody was HRP-conjugated anti-IgG of the appropriate species (Jackson ImmunoResearch Laboratories) at 1:1000 dilution.

Telomerase assay

Telomerase activity of the primary cells and the immortalized cells was measured with TRAP (telomere repeat amplification protocol) assay using the TRAPEZE XL Telomerase Detection Kit (Millipore) according to the manufacturer's instructions. The values for total products generated

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(TPG), which represents telomerase activity, were obtained from three independent experiments and expressed as a mean \pm SEM.

TEER and transport of radiolabeled substrate

Transepithelial electrical resistance (TEER) was first used to assess the adequacy of the epithelial monolayer in the Transwell culture system, and then radiolabeled carboxyl ^{14}C -inulin (MP Biomedicals) was used to measure paracellular transport properties of immortalized rat arachnoid cells, as an indirect measure of tight junction formation and presumed blood-CSF barrier properties. Because arachnoid primary culture cells did not readily grow to confluence, it was not possible to compare directly with the immortalized cells. Caco-2 epithelial cells were used as an internal control, since reference values are available. Caco-2 cells were obtained from American Type Culture Collection (Rockville, MD, USA) at passage 18. DMEM with FBS as described above was applied to apical and basal portions of the Transwell system for arachnoid cells and allowed to equilibrate for 2 h in a CO_2 incubator before fresh media was added and cells were seeded. Immortalized DT rat arachnoid cells at P70 and Caco-2 cells at P24 were plated in media at density 1×10^5 cells/ cm^2 in 12-well plates with collagen-coated PTFE Transwell inserts (Corning Cat. #3494). Transwells without cells (blank) were used as a control, and naive rat cells were also plated at density 1×10^6 cells/ cm^2 for comparison. After growth to confluence, the transepithelial membrane resistance (TEER) was measured with an epithelial voltmeter (World Precision Instruments) according to the manufacturer's recommendations. For radiolabeled transport studies, we used ^{14}C -inulin in the range of 10 nM–6 μM for linear non-concentration dependent transport [146]. ^{14}C -inulin stock solution at specific activity of 2.38 mCi/g was prepared as 1 μl radiolabeled solution per 1000 μl assay buffer, for inulin concentration 21 $\mu\text{g}/\text{ml}$ and specific activity 0.05 $\mu\text{Ci}/\text{ml}$. Buffer was removed from the apical compartments and 1 ml of pre-warmed radioactive solution was added to each apical chamber, being careful not to spill into the basolateral chamber. The plate was put onto a gentle shaker at 37 $^\circ\text{C}$ and 100 μl samples were taken from both compartments in each well at 0, 15, 30, 60, 90, 120 min and replaced with equal volumes of respective buffer. Counts were measured in a scintillation counter and transport was expressed as the apparent permeability coefficient P_{app} using the standard transport formula $P_{app} = dQ/dt [1/(AC_0)]$ where dQ/dt is the steady state flux, A is the

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surface area of the Transwell in cm^2 , and C_0 is the initial concentration in the apical portion of the Transwell [147],[148].

Three-dimensional culture system and scanning electron microscopy (SEM)

For SEM, arachnoid cells at P76 at an optimal density of $75,000 \text{ cells/cm}^2$ were seeded onto a collagen matrix consisting of bovine type I collagen (Devro, Somerville, NJ, USA) which was manufactured according to a standard protocol [108], in DMEM media with 10% FBS as described above. We utilized a range from $25,000$ to $175,000 \text{ cells/cm}^2$ for immortalized cells until this optimal seeding density was determined. After growth for 10–12 days, the media was aspirated and the collagen support was washed with PBS and the samples were then fixed en bloc in 2.5% glutaraldehyde, passed through a standard series of ethanol–water mixtures to absolute ethanol, and dried using an EMS 850 critical point dryer. A sputter coater was used to coat dried sponges with a 10 nm gold layer and a Hitachi S3500N variable pressure SEM was used to capture images of the samples. For better visualization of cells, false color was applied to selected images.

Karyotyping

Karyotype analysis was performed in order to determine the extent of structural changes after viral transduction. We predicted that the karyotype would show changes from normal diploid state following immortalization, but the extent of karyotypic change after viral transduction was unknown. After a 3.5 h colcemid treatment, cells were harvested according to standard cytogenetic protocol (University of Minnesota Cytogenetics Core Laboratory). The resulting metaphase cells were evaluated by G-banding and more than 15 metaphases were completely analyzed in ST and DT cells.

Results

The aim of this study was developing and partially characterizing immortal arachnoid cell lines which could be utilized for physiological studies in modeling normal CSF flow, and which could be modified or treated with various substances to study pathological conditions such as hydrocephalus, arachnoid cysts, or other disorders. As a starting point, the following basic facts needed to be established: (1) that the cells had been stably transduced with the intended gene constructs; (2) that the cells retained normal immunohistochemical and morphological

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phenotypes of arachnoid cells, including the ability to form an intact epithelial monolayer with essentially normal physiology; (3) that the cells displayed the expected behavior of immortalized cells, such as rapid and sustained cell division through many passages. As described below, our results support an immortalized arachnoid phenotype which is nevertheless identical to normal arachnoid cell morphology, immunohistochemical profile, and key growth properties including contact inhibition and basic epithelial barrier formation. Immortalized cells have not exhibited evidence of whorls, calcification, or typical histopathology seen in meningiomas.

Rat arachnoid cells were stably transduced with SV40 LTA_g and hTERT

After treatment of the primary rat arachnoid cells with retroviral vectors, the resultant immortalized cells were subjected to antibiotic and growth-dependent selection. Efficiency of viral transduction with pBABE-puro-SV40LT and pBABE-neo-hTERT was confirmed by immunofluorescence and Western blotting using antibodies against SV40 LTA_g and hTERT. Both ST and DT cells at early and intermediate passages showed stable expression of SV40 LTA_g that localized in the nucleoli of immortalized cells, and a 82 kDa band corresponding to SV40 LTA_g was detected by Western blotting in cell extracts (Fig. 3.1A). hTERT protein was visualized in nucleoli of DT cells, as well as in the cytoplasm due to very high expression levels, and a 122 kDa band corresponding to hTERT was detected by Western blotting in nuclear extracts. HeLa nuclear extract was used as control for hTERT expression (Fig. 3.1B).

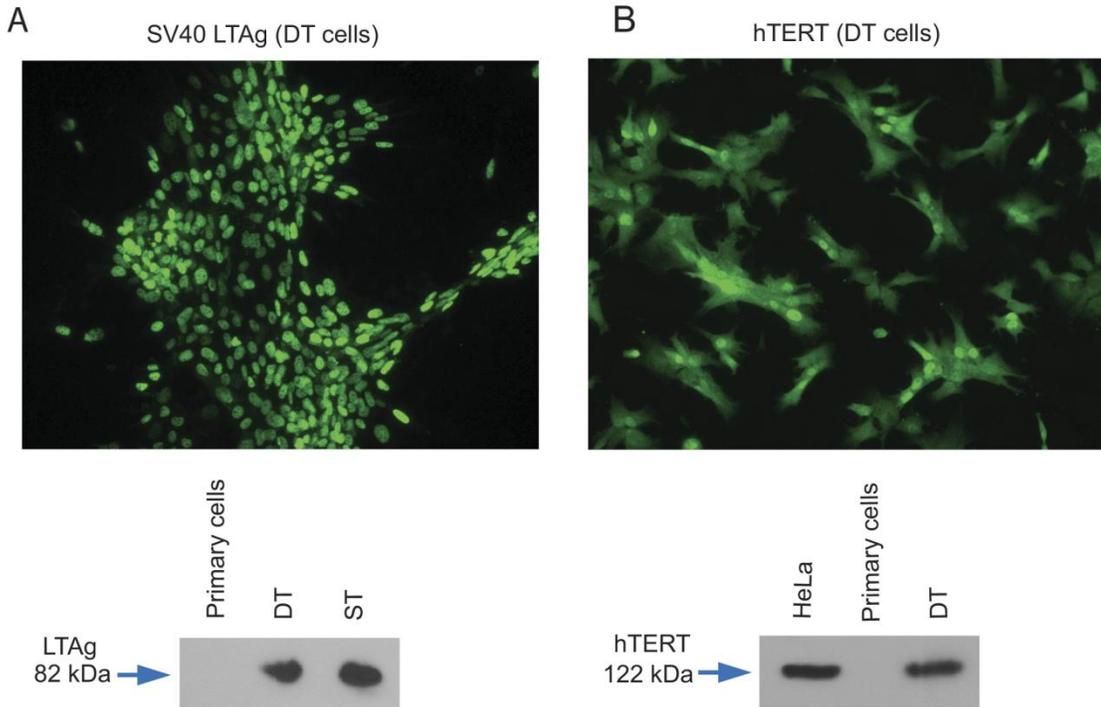


Figure 3.1. Expression of SV40 LTA and hTERT in immortalized arachnoid rat cells. After transformation with SV40 LTA or SV40 LTA+hTERT, arachnoid cells were cultured and seeded for immunostaining *in situ*. Total protein extracts were also prepared from the same cultures for Western blot analysis. Commercial primary antibodies against SV40 LTA and hTERT were used for detection. (A) Double-transduced, immortalized cells at early passage, showing immunofluorescence staining for SV40 LTA, with confirmation of a 82 kDa specific band for LTA in ST and DT cells by Western blot. As expected, SV40 LTA protein is localized in the nuclei. (B) Double-transduced, immortalized cells at early passage, showing immunofluorescence staining for hTERT, with confirmation of 122 kDa specific band for hTERT in DT cells. HeLa cells represent a positive control for expression of hTERT and native cells represent a negative control.

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Immortalized cells maintained morphology and expression of epithelial markers

A key question to address was whether the immortalized arachnoid cells would retain the phenotype of native cells, including the expression of the epithelial markers which have been shown collectively to define the phenotype [32],[149],[33]. In addition, cell morphology and growth properties were primary endpoints we examined in order to confirm that transformed cells retained the phenotype of native cells and could be used for future physiological experiments involving membrane flux, with an assumption of equivalence.

Both ST and DT immortalized arachnoid cells exhibited morphology which was identical to the original primary arachnoid culture. Immortalized cells at early and late passages displayed spindle-like appearance at low density before reaching confluency and “cobblestone” appearance after becoming fully confluent, which appeared identical to early passage primary cells (Fig. 3.2). In addition, we tested a panel of immunohistochemical markers, which were previously shown to define the arachnoid cell phenotype [32],[149],[33]. Phenotype of ST and DT cell lines was verified by immunofluorescence staining with antibodies against cytokeratin, desmoplakin and vimentin. Strong immunohistochemical signal was observed both in ST cells (Fig. 3.3) and DT cells (data not shown) at early and intermediate passages. Western blotting also was performed at early (P10) and late (P160) passages to confirm stable expression of these protein markers in both immortalized cell lines. Bands of expected size were detected for vimentin, cytokeratin and desmoplakin in ST cell extracts (data not shown) and DT cell extracts (Fig. 3.3). The same phenotype and expression of protein markers was present at early (<20) and late (>160) cell passages and was not affected by thawing after storage in liquid nitrogen.

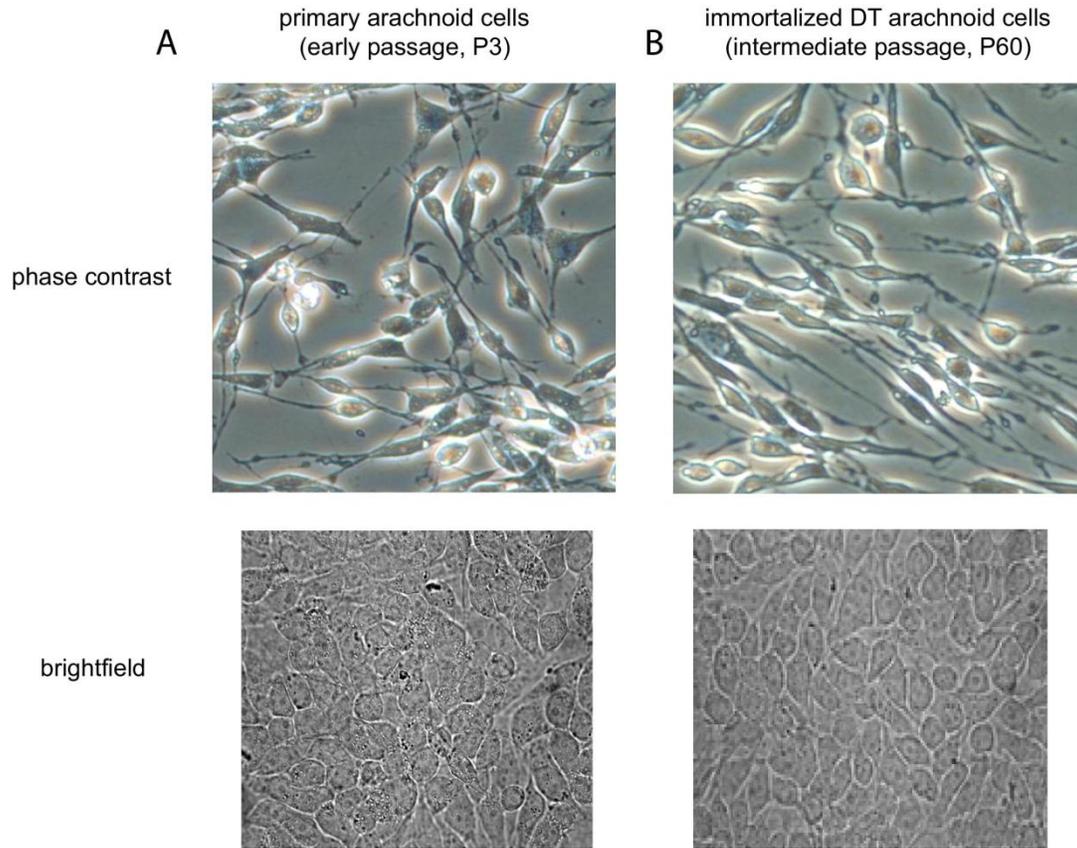
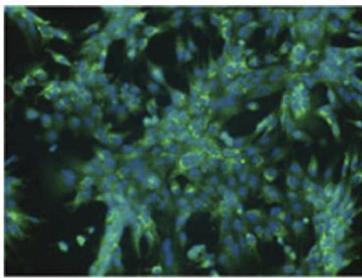
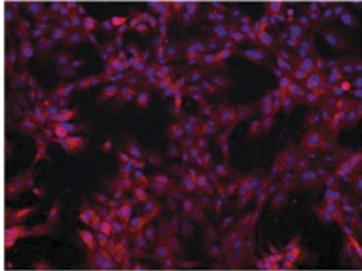
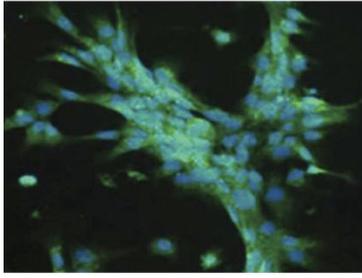


Figure 3.2. Morphology of native and immortalized rat arachnoid cells. Primary cells at P3 and immortalized DT arachnoid rat cells at P60 were maintained in culture and observed at different passages and stages of confluency. Top panels show phase-contrast microscopic images before confluency with typical spindle-shape appearance, with early passage primary (A) and intermediate passage immortalized DT cells (B) showing the same morphology. Bottom panels show brightfield microscopic images demonstrating “cobblestone” shape and contact-inhibited growth in the same culture, with a selected area of early passage primary cells able to grow to confluence; this ability was lost in later passage cells. The double-transduced immortalized cells show conservation of morphological features of primary rat arachnoid cells both before and after reaching confluency (top and bottom images respectively).

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A



B

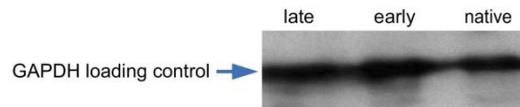
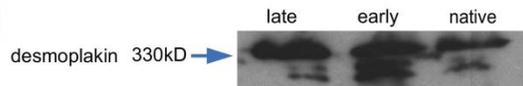
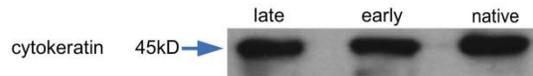


Figure 3.3. Immortalized rat arachnoid cells express characteristic epithelial markers. Stability of expression of protein epithelial markers vimentin, cytokeratin and desmoplakin in immortalized ST and DT cells was confirmed by immunostaining *in situ* and Western blots. (A) Immunofluorescence staining of P20 single-transduced (ST) immortalized cells, with specific antibodies against vimentin, cytokeratin, and desmoplakin. Similar staining patterns were seen with intermediate and late-passage ST and DT cells. (B) Expression of vimentin, cytokeratin and desmoplakin detected by Western blot in native arachnoid cells, double-transduced early passage, and double-transduced late passage. GAPDH staining was used as a loading control. Estimated molecular weights for each protein are indicated.

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Expression of LTA_g and hTERT significantly increases telomerase activity in immortalized rat arachnoid cells

Because the level of native rTERT was formerly unknown in primary arachnoid cells, we sought to quantify the level of native rTERT and also to determine whether the level of native telomerase activity was significantly affected by SV40 LTA_g. We began by confirming the immunohistochemical presence of telomerase and then quantified enzymatically active telomerase with a standard TRAP assay, which was performed on naive, ST, or DT cells.

Telomerase activity is expressed in units of TPG where one unit corresponds to the number of “TS primers” extended with at least three telomeric repeats in extract in 30 min at 30 °C during the assay. We found that telomerase activity was 7.1 ± 0.6 for primary cells, 12.1 ± 0.3 for ST and 16.9 ± 0.4 for DT cells (Fig. 3.4). These results indicate that primary rat arachnoid cells have a low baseline level of rat telomerase activity, which was significantly increased by expression of SV40 LTA_g and/or hTERT. Of note, the SV40 LTA_g alone was sufficient to increase native rat telomerase significantly, in this case 1.7-fold over endogenous rat telomerase activity.

Additional transduction with human telomerase further increased total telomerase activity to 2.4-fold. Although wild-type cells already had some endogenous rat telomerase activity, it is important to note that they grew senescent over five doubling times.

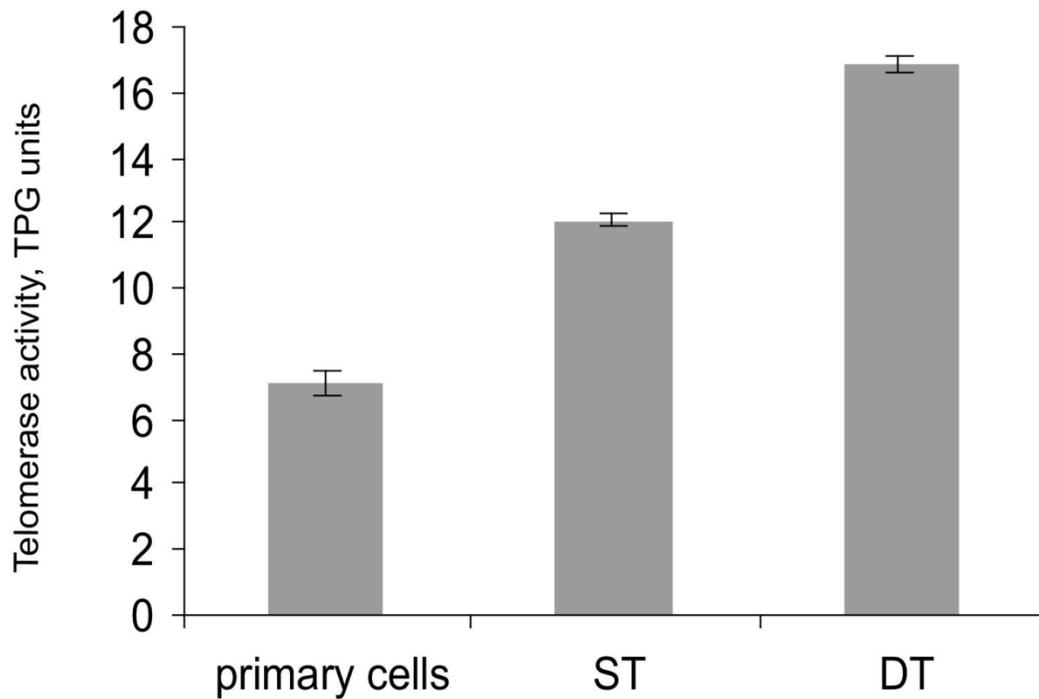


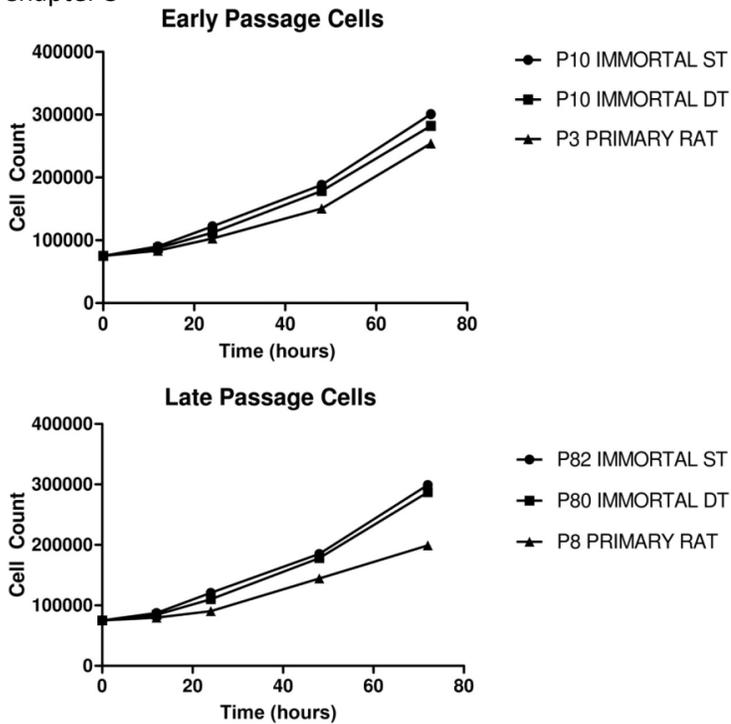
Figure 3.4. Expression of LTA_g and hTERT increases telomerase activity in rat arachnoid cells. Protein extracts were prepared from primary cells, ST and DT cells. Relative telomerase activity was measured in cell extracts using the TRAP assay. Telomerase activity is expressed in TPG units where one unit corresponds to the number of telomeric specific primers extended with at least three telomeric repeats. The values represent the means of three different experiments and error bars show \pm SEM. The differences between all values are statistically significant ($P < 0.05$).

Growth of immortalized arachnoid cells is superior to native cells

Despite the DT cells having significantly higher telomerase than ST cells, we found that the DT cells were nearly equivalent in their growth profile. Because the defining feature of immortalized cells is continued, stable growth under culture conditions, we characterized the growth properties of ST and DT cells by doubling time measurements at early and late passages. In the past, arachnoid cell lines which were initially presumed to be immortal were found to undergo senescence or other phenotypic changes at P50 or earlier [97].

Fitting the data to a standard exponential growth model, we found that the doubling time in two-dimensional culture plates was significantly decreased in ST or DT arachnoid cells compared to native cells at both early and late passages ($P < 0.001$), and there was also a small but statistically significant difference in doubling time between ST and DT cells at both early and late passages ($P < 0.001$), with the ST cells growing slightly faster (Fig. 3.5). We found that this small difference in doubling time between ST and DT made no practical difference in culture technique, however, and ST and DT cells behaved equivalently at the early, intermediate and late passages out to P160. There was a non-statistically significant difference between doubling time in early vs. late passage ST and in early vs. late passage DT cells, but there was a highly significant difference ($P < 0.001$) between early and late passage native cells, which is consistent with their known senescence after approximately P8.

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Cell Type	Doubling Time (h)	95% CI
ST immortal, early passage	35.7	34.5 - 36.9
DT immortal, early passage	36.4	35.3 - 37.7
Native, early passage	37.8	35.1 - 40.8
ST immortal, late passage	34.5	33.8 - 37.2
DT immortal, late passage	35.3	33.9 - 36.7
Native, late passage	46.7	43.4 - 50.6

Figure 3.5. ST and DT immortalized arachnoid cells show enhanced replicative capacity. Population doubling time of ST and DT cells were compared to primary rat arachnoid culture at early and late passages. The growth rate of each cell culture was determined as an increase in cell number over the course of 72 h. All counting experiments for each cell line were done in triplicate. The error bars are not visible on the scale of the graph due to small size. As noted in the text, there was no significant difference between ST cells at early vs. late passage and no difference between DT cells at early vs. late passage. As expected, however, the difference in doubling time between native cells at early vs. late passage were highly significant, as was the difference in doubling time between the native cells and immortalized cell lines.

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Seeding capability in three-dimensional collagen matrices was also measured qualitatively with wild-type primary cells and immortalized cells. Using scanning electron microscopy (SEM), we found that ST or DT cells at early (P10) and intermediate (P50) passages densely populated the collagen matrix at an initial seeding density of 7.5×10^3 cells/ml (Fig. 3.6) compared to wild type cells which were senescent prior to even approaching confluence and were therefore unsuitable for seeding collagen sponges. The initial density of seeding of native cells did not appear to affect this obvious deficiency of non-immortalized cells; even when seeded at an increased density of up to 2.5×10^5 cells/ml the non-immortalized cells did not demonstrate any growth approaching confluence on the three dimensional matrix.

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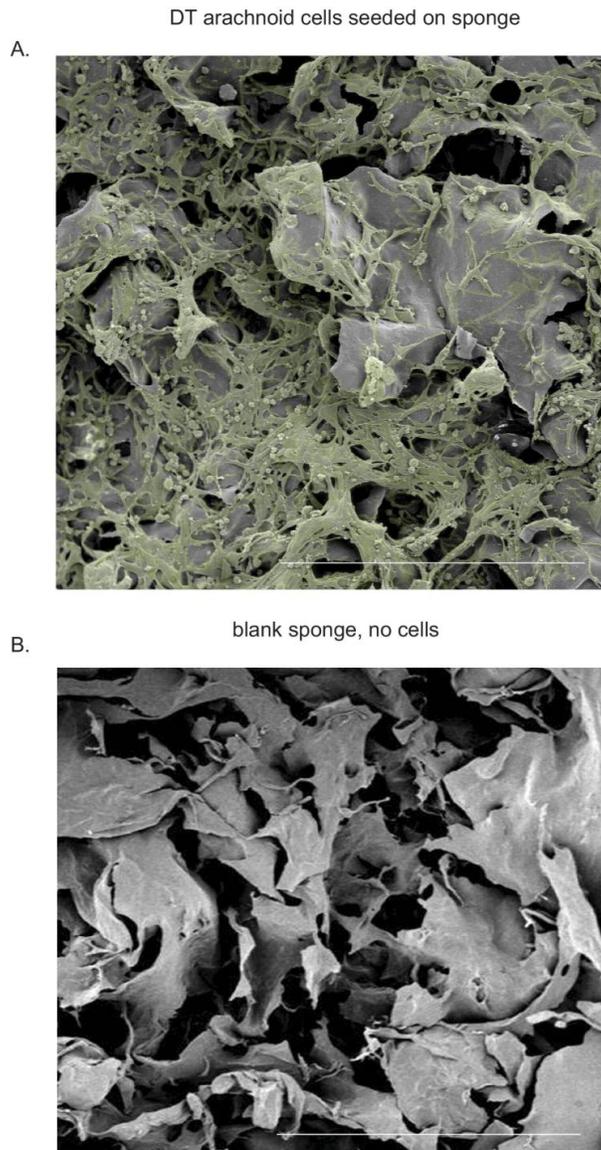


Figure 3.6. Immortalized cells exhibit enhanced capacity for growing on three-dimensional support. Immortal ST arachnoid cells were seeded onto a collagen matrix sponge and grown *in vitro*. (A) Scanning electron micrograph of immortalized rat arachnoid culture on sponge with green false coloration. (B) Control blank sponge for comparison, without cells seeded. Primary cells seeded onto sponges showed very sparse growth and

qualitatively did not approach confluence (data not shown), with an appearance similar to a blank sponge, irrespective of seeding density. Bar=500 μ m.

Membrane properties indicate an intact epithelial monolayer

In order to verify the structural integrity of our epithelial monolayer and provide supportive evidence for tight junctions or desmosomes, TEER was directly measured in arachnoid cells and in Caco-2 cells, a widely used model of paracellular epithelial transport which reliably forms tight junctions [146]. In both cases, TEER was consistent with an intact epithelial barrier. For Caco-2 cells the TEER depends on the cell line and culture model but is typically 150–600 $\Omega\cdot\text{cm}^2$ [150], with one recent source reporting a typical TEER value of $260\pm 65 \Omega\cdot\text{cm}^2$ [148] for early passage cells. For type II MDCK cells, another cell line commonly used in studies of tight junctions and epithelial transport, reference values for TEER are 200–300 $\Omega\cdot\text{cm}^2$ [146]. Because TEER is dependent upon a closed epithelial barrier of confluent cells, our non-transformed primary arachnoid cells did not grow adequately on Transwell membranes in order to assess TEER, and those values were indistinguishable from a Transwell membrane without cells, $110\pm 3.5 \text{ SEM } \Omega\cdot\text{cm}^2$. TEER values of confluent immortalized arachnoid cells, adjusted for membrane resistance, was $193\pm 10 \text{ SEM } \Omega\cdot\text{cm}^2$ and $206\pm 14 \text{ SEM } \Omega\cdot\text{cm}^2$ for Caco-2 cells plated under the same conditions at density $1\times 10^5/\text{ml}$, which is within the published reference range.

After assessing the basic integrity of the monolayer, we proceeded to assess paracellular or transcellular transport properties in the two-dimensional Transwell culture system using a radiolabeled ^{14}C inulin assay. In an experiment directly comparing arachnoid cells to Caco-2 cells, the intermediate passage immortalized DT arachnoid cell P_{app} was 8.6×10^{-6} with 95% CI $\pm 3.6\times 10^{-6}$ and the Caco-2 cell P_{app} was 8.8×10^{-6} with 95% CI $\pm 3.7\times 10^{-6}$, suggesting paracellular transport is blocked by confluent arachnoid cells or Caco-2 cells, and barrier properties were not significantly different under identical conditions at confluence. These values are in accord with reference values of similarly transported substances for Caco-2 cells. For example, the typical P_{app} for mannitol or inulin solution for Caco-2 cells is in the $10^{-6} \text{ cm}^2/\text{s}$ range [150],[148]. The plot of dpm vs. time (Fig. 3.7) expressed as a concentration ratio $[C_{\text{basal}}]/[C_{\text{apical}}]$ for arachnoid vs. Caco-2 cells shows clear divergence in slopes with respect to control and a non-significant

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difference in slopes between arachnoid and Caco-2 cells ($P < 0.13$), which suggests that the transport behavior of the cell monolayer is very similar. While electron microscopic evidence of tight junctions and further examination of transport properties for other substances will be necessary for further characterization, these data strongly support the presence of an intact epithelial monolayer.

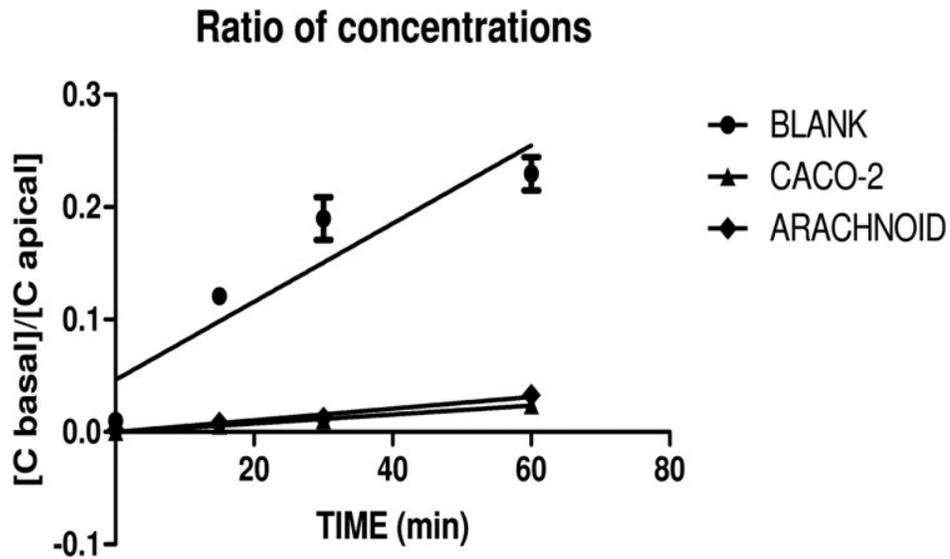


Figure 3.7. Radiolabeled transport study.

^{14}C inulin was used to test paracellular transport in immortalized arachnoid cells compared to Caco-2 cells. Due to poor growth on the Transwell supports, primary arachnoid cells were indistinguishable from blank wells on preliminary TEER studies and are not included in this analysis. We found equivalent slopes for confluent arachnoid and Caco-2 cells, which together with TEER data suggest that the membrane has limited permeability to paracellular transport.

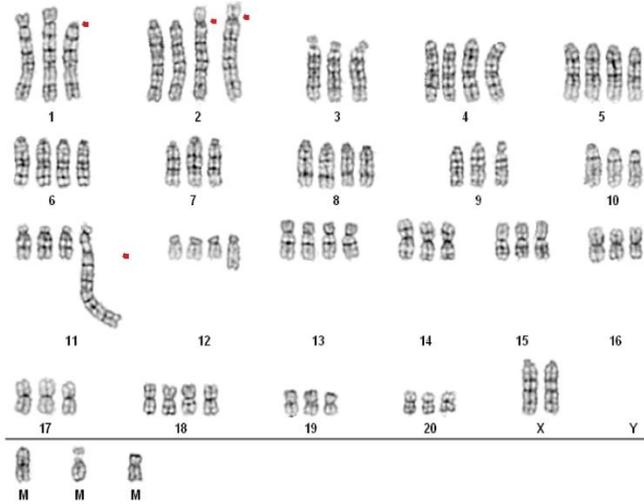
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Karyotype analysis of immortalized arachnoid cells

To assess the genomic stability of the single and double transduced cells, especially given the high multiplicity of infection, we performed karyotyping analysis. We expected some chromosomal rearrangements from the normal 21 pairs of rat chromosomes, as well as potential differences between ST and DT cells. Karyotyping indicated a single, near-tetraploid clone in ST cells, consisting of 75–78 chromosomes. The karyotype is 75–78,XX,-1,del(1)(p11),add(2)(p11)x2,-3,-7,-9,-10,der(11)t(2;11)(q11;q23),-14,-15,-16,-17,+3-4mar. Relative to a pure tetraploid complement, with four copies of chromosomes one through 20, there was loss of one copy each of chromosomes #3, 7, 9, 10, 14, 15, 16 and 17. Structural abnormalities included a deletion of the short arm of one chromosome #1, additional material of unknown origin added to the short arms of two #2 chromosomes, an extra copy of the long arm of chromosome #2 translocated to the distal long arm of a chromosome #11, and three small marker chromosomes of unknown origin. In DT cells two related clones were present. Clone 1, corresponding to the ST clone above, comprised 67% of metaphase cells tested (Fig. 3.8A). Clone 2, comprising the remaining 33% of metaphases, had the same abnormalities as Clone 1, and in addition, a dicentric chromosome joining together the proximal short arms, centromere, and long arms on one X and chromosome #2 in place of one X chromosome and one chromosome #2, and deletion of part of the long arm of one chromosome #5 (Fig. 3.8B). Additionally, in place of one normal chromosome #1 was a chromosome #1 with an apparent large homogeneously staining region (HSR). Such HSR typically represent a region of gene amplification. Clone 1 is the same as that detected in the ST line, but Clone 2 demonstrates cytogenetic evolution.

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A. Clone 1, 100% of metaphase ST cells, 67% of metaphase DT cells



B. Clone 2, 33% of metaphase DT cells

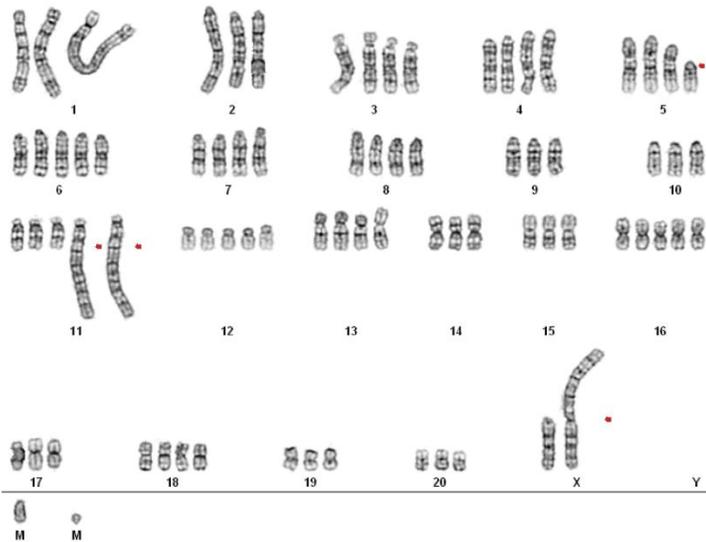


Figure 3.8: Karyotype analysis. Immortalized cells showed a near tetraploid karyotype with a number of stable chromosomal abnormalities, as opposed to normal diploid rat karyotype which contains 21 pairs of chromosomes. Normal karyotype of native cells was verified (data not shown). Many immortalized cell lines are tetraploid or near-tetraploid. Both clones had small marker chromosomes (“M”) of unknown origin and significance, though these are occasionally associated with virally transformed rat cells [151].

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Discussion

In this study, we report the first immortalization of primary arachnoid cells, as an initial step toward manufacture of arachnoid cell bioscaffolds for modeling cellular transport properties. We utilized both a one-step and a two-step retroviral transduction with LTA_g and hTERT. If desired, the two-step approach can be adapted to human source material with amphotropic MMLV-based viral packaging. Irrespective of approach, we observed similar functional properties of the ST and DT cells, which were clearly superior to native arachnoid cells in doubling time and their ability to establish a confluent monolayer while maintaining a normal phenotype.

Native rat arachnoid cells have a baseline level of rat telomerase activity which was significantly increased by transduction with LTA_g, and additional human telomerase did not change the phenotype or augment the growth rate from the changes induced by LTA_g, and in fact may have lengthened it slightly. These results confirm prior reports that telomerase expression is permissive in rodents [122], including the rat, and also suggest that telomerase is important for immortalization in rat cells but it is not necessary to achieve the highest possible levels of telomerase, perhaps only a threshold amount, in order to bypass senescence. Other investigators [131] reported that double-transduced cells (SV40 LTA_g+hTERT) had a shorter doubling time than single-transduced cells (hTERT) in human meningioma cells. Our doubling time for both ST and DT cell lines (<36 h) was considerably shorter than immortalized DT human cells, which in the best case were 96 h [131], which could be a species specific feature or alternatively, could be a result of extremely high levels of expression of the LTA_g transgene.

Both ST and DT arachnoid cell lines stably express a combination of epithelial markers specific to arachnoid cells, are capable of forming monolayers with restricted epithelial membrane transport, and were able to grow on collagen sponges as well as two-dimensional membranes. As a neural ectoderm derived tissue, the cells showed a high-level of cytokeratin and vimentin intermediate filament expression at both early and late passages, and also demonstrated expression of desmoplakin, an essential component of desmosomes. The immortalized cell lines both showed extensive karyotypic changes post-transduction, including a near-tetraploid

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karyotype which is not unusual in transformed or cancer cells. In functional terms, there is no obvious link between the observed aneuploidy and any specific gene loci, such as homologs of NF2 on rat chromosome 14 and Rb on rat chromosome 15, and we have not performed any more detailed characterization at the individual gene level.

Membrane transport properties of arachnoid cells are not currently well-known, but it is thought that transcellular and paracellular transport occurs through these cells with an intact CSF-blood barrier. We found indirect evidence of epithelial tight junctions with TEER and radiochemical data, with a cellular membrane resistance similar to Caco-2 cells, as well as an immunohistochemical pattern suggesting desmosomes, but further work will be needed to characterize the cell membranes with transmission electron microscopy. Modeling of microscopic arachnoid villi *in vitro* will provide a unique system for studying transport properties of arachnoid cells and understanding molecular mechanisms of water flux and solutes along with related clinical problems. Planned techniques for studying arachnoid transport include Raman spectroscopy and vesicular labeling with radiolabeled substrates in two-dimensional Ussing chambers. It is hypothesized that our three-dimensional system also will provide a more physiologically relevant model of water and ion flux than standard two dimensional models. Although other models currently exist for studying arachnoid pathophysiology, including meningioma tissue and cell lines, stable arachnoid cell lines permit study not only of the normal arachnoid physiology but also (by chemical treatment or adaptation of our immortalization methods to genetically engineered animals) provide a potentially more physiologic method to study hydrocephalus and other abnormal processes. Aside from understanding details of water and solute transport in arachnoid granulations, our ultimate goal is to create a bioartificial shunt using immortalized cells on a collagen scaffold, which could replicate properties of normal arachnoid cells and might obviate the need for CSF shunting in hydrocephalus.

Chapter 4: The Characterization of Arachnoid Cell Transport: Paracellular transport and Blood CSF Barrier Formation of Arachnoid Cells

Defining barriers: the Paracellular Transport of Arachnoid Cells

Perhaps the most two most important role for arachnoid cells are the formation of the blood CSF barrier isolating the brain from the remainder of the body, and the removal of CSF and other substances out of the brain. These two tasks are related in that any barrier demands that certain substances are selectively transported. For almost all substances, barrier transport implies passage through either transcellularly, paracellularly, or in sparsely populated tissue, through extracellular matrix. Barriers may be defined in a number of ways: the hydrophobicity, the size, the origin, or a number of other characteristics of the substance being moved. The blood brain barrier traditionally has been defined by size, but within the scheme of cellular mechanisms of transport, its stratification does not shed light on how substance transport except in the context of sieves with measurable pore size. This is particularly true in light of current concepts of the blood brain barrier where multiple layers and multiple cell types may play a role in admittance of substances into the brain. The blood CSF barrier however is simpler, with the cell types more uniform. Yet their geometry indicates a variety of mechanisms may be at play. We therefore broke down the various mechanisms of transport and focused on paracellular movement in this chapter. Not only is it likely the dominant means by which CSF transfer to the vascular compartment, it most likely is responsible for the classical size differential character in barriers.

The work is carried out by Eric Hansen, Christopher Janson, Alexander Bryan, and Cornelius Lam. The manuscript is written by Cornelius Lam

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Introduction

Cerebrospinal fluid (CSF) is important for the central nervous system's support and maintenance. It buffers the nervous tissues mechanically and chemically, serves as a vehicle for the transport of important substances, and removes waste and debris.[152] Arachnoidal CSF egress is considered one of the major routes of CSF removal. [31] How this occurs is unknown, but given the aqueous nature of CSF, the primary mean is thought to be paracellular. As a major component of the blood-CSF-barrier (BCB) and sink to the CSF, the arachnoid stands at the junction between the vascular system and the intracranial space. This gateway is similar to the blood brain barrier in that polar substances are restricted in their movement [153]. Arachnoidal tissue exists in multiple forms including membranes, dense granulation caps, and porous central cores. The degree of intracellular or extracellular matrix pathway involvement is probably dependent on this local structure of the arachnoid tissue, but preliminary tracer studies have shown that permeabilities of low molecular weight substances in monolayers parallel that of the blood brain barrier.[36] [154] Tight junctions crucial to the integrity of the BCB and regulation of paracellular transport have been seen in arachnoid cell-cell contacts with transmission electron microscopy.[155] Holman recently demonstrated these junctional complexes on cultured arachnoid monolayers as well. These complexes maintain pathway integrity in conditions of osmotic and pressure gradient challenges. The geometric path in the paracellular space could be altered during these conditions, regulating the outflow of fluid out of the brain and intracranial cavity probably by a combination of complex feedback systems involving second messengers and physical alterations in the cells.

Because of the similarities in permeabilities of ionic substances in arachnoid cell mediated blood CSF barrier and blood brain barrier (BBB), the demonstration of regulated flow in arachnoid cell, and the importance of arachnoid cells in the removal of cerebrospinal fluid from the brain, we characterize the paracellular transport in an immortalized cell line of arachnoid cells developed in our laboratory (see [156] for cell line description) and investigate the physiologic mechanisms that alter this transport in this paper. Two important mechanisms in tight junction regulation are the calcium and cAMP second messenger pathways.[157][158] They regulate the various intercellular junctional proteins, such as claudin, as well as intracellular systems important for

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transport. Given the cell's barrier capabilities, we expect the molecular dynamics to be similar to the blood brain barrier. However, an overarching element of contrast however between arachnoid cells and brain endothelial cells is that the "neurovascular unit" is absent (see [159] for review). Lacking the astrocytic, neuronal, and pericytic influences in the BBB junctional complex, we believe the mechanisms of the BCB maintenance to be under different control and regulation. To that end, we believe the control mechanisms to be simpler and to be less finely controlled.

Methods

Production of retrovirus containing SV40 LgTA_g and hTERT and retroviral transduction

The generation of immortalized arachnoid cells has been previously presented.[156] Briefly, retroviral constructs pBABE-neo-hTERT and pBABE-puro-SV40LT, containing hTERT and SV40 LTA_g along with the G418 and puromycin resistance genes, were obtained. The purified plasmids were then used to transfect EcoPack2 cells (Clontech), which are 293HEK ecotropic feeder cells containing retroviral packaging genes. Cells were seeded 12-18 hrs prior to use at 5×10^5 cells in 25 cm² flasks. Then 5mg of pBABE-puro-SV40LT was combined with Fugene reagent (Roche) and OptiMem (Invitrogen) serum-free media in 250 ml total reaction volume with 3:1 ratio of Fugene:DNA. This was incubated for 30 min and added to each flask of 293HEK ecotropic feeder cells, with 3ml of serum-containing media per flask.

Arachnoid cells were harvested from 21-23 day old male Sprague-Dawley rats. At passage 3 or 4, the arachnoid cells were replated into a Biocoat six-well plate (BD Biosciences). Viral transduction was performed when the cells reached 60-80% confluence. Clarified viral supernatant containing BABE-puro-SV40LT was applied sequentially to the arachnoid cell primary culture. Target cells were initially at a density of 4×10^4 cells per well of a six-well plate. The media was aspirated and 3 ml virus-containing media was added per well. Polybrene (Millipore) was then added to a final concentration of 4 mg/ml. Cells transduced with pBABE-puro-SV40LT were selected over 14 days with puromycin (Sigma).

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Functional transport assay: TEER, marker, and size differential transport study

4×10^5 immortalized rat arachnoid cells were plated in each of the 3 top wells of a 6-well Transwell plate (Corning Inc. Corning, NY; Cat no. 3450) (4.67cm^2 per well and $0.4 \mu\text{m}$ pore size), and incubated for 3-5 days depending on when the cells became confluent. The 3 bottom (blank) Transwells were used as a negative control. A separate 24-well plate Transwell (Corning Inc. Corning, NY; Cat no. 3470) (0.3cm^2 per well and $0.4 \mu\text{m}$ pore size) was used for TEER studies. Cells were plated at 3×10^4 cells per well and grown to confluency. Culture media in Transwell plates was removed and pre-warmed media was added into wells (apical 2 ml, basolateral 3 ml). The ^3H -mannitol stock solution was prepared as 1ml radiolabeled mannitol per 1000 ml of assay buffer [LR1], for a final mannitol concentration of 82nM and specific activity 1 mCi/ml. Buffer was removed from the proximal (apical) compartments and pre-warmed radioactive solution was added to apical chambers, with 2 ml to each chamber. The plate was put on gentle shaker at 37°C and $200 \mu\text{l}$ samples were taken from both compartments in each well at 15, 30, 60, 90, 120 minutes and replaced with an equal volume of respective buffer. Inulin-[Carboxyl- ^{14}C] (50 mCi/mmol, Fisher Scientific Inc. Cat #1108650) and [^{14}C] Urea (54 mCi/mmol, Amersham, Piscataway NJ) were prepared as 1 ml of radiolabeled inulin per 1000 ml assay buffer. For the FITC labeled Dextran (10, 40, and 70 kilodaltons) (Cat no. 129K5304, 83797PJ, 069K5316. Sigma-Aldrich Co., St. Louis, MO) experiment, 1×10^5 immortalized rat arachnoid cells were seeded and tested in a similar manner. All signals were measured using a Packard SpectraCount photometric microplate reader (measured at 520 nm)(Packard Instrument Co., Meriden, CT) with control plates subtracted out. TEER studies were performed using a transepithelial voltmeter (World Precision Instruments) according to the manufacturer's recommendations.

The amount of tracer crossing the monolayer was reported as arachnoid permeability ($P_{\text{arachnoid}}$, cm/s). The cleared volume was calculated by dividing the concentration in the receiver compartment by the product concentration in the donor compartment at each time point. Average cumulative volume cleared was plotted versus time and the slope was estimated by linear regression analysis to give the mean and the standard deviation of the estimate. The P value for the arachnoid monolayer alone was obtained as follows: $1/P_{\text{arachnoid overall}} = 1/P_{\text{(recorded)}}$ -

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$1/P_{\text{insert}}$. To generate the permeability coefficient of arachnoid cells, $P_{\text{arachnoid}}$ (cm/sec), $P_{\text{arachnoid}}$ overall value were divided by the surface area of the insert.

Theoretical pore size for neutral permeants was determined using the Renkin molecular sieving function, which uses the molecular radius (r) of the tracer and a cylindrical pore radius to model the paracellular space. [160] The molecular radii are estimated using the Stokes-Einstein Law for equivalent spheres, which for mannitol and urea radii are 4.10 and 2.67 Å respectively. Solute pairing allows for aqueous pore radius calculation for paracellular permeability ratio thus:

$$\frac{P_x}{P_y} = \frac{r_y F\left(\frac{r_x}{R}\right)}{r_x F\left(\frac{r_y}{R}\right)}$$

where the hindrance function is defined thus:

$$F\left(\frac{r}{R}\right) = \left(1 - \left(\frac{r}{R}\right)\right)^2 \left[1 - 2.104\left(\frac{r}{R}\right) + 2.09\left(\frac{r}{R}\right)^3 - 0.95\left(\frac{r}{R}\right)^5\right]$$

Pore occupancy to length ratio (ϵ/L) as a characteristic value of the theoretical pore size is calculated using mannitol and urea using this equation [161]:

$$P_x = \frac{\epsilon}{L} D_x F\left(\frac{r_x}{R}\right)$$

Where D is the diffusion coefficient and subscript, x , indicates either mannitol or urea.

Perturbation methods

Second messengers, Calcium

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Extracellular calcium was investigated using ethylenediaminetetraacetic acid, EDTA (MP Biomedicals, Solon, OH), as a chelator at 20mM concentration. Permeability studies were performed at maximal effective dose as determined by dose response curve for the arachnoid cells at 15 minutes after treatment initiation. Dosing and timing for transport studies was determined from temporal data gathered from serial TEER values measured at 5 minute intervals for 90 minutes at concentrations of 1, 5, 10, 20, and 40 mM EDTA. Calcium was also increased in culture media to a concentration of 4mM from 1.8 mM. Intracellular calcium was perturbed in two ways. Intracellular calcium was decreased by using the calcium channel blocker, verapamil (MP Biomedicals, Solon, OH), at a concentration of 5 μ M.[162] Intracellular calcium was also increased by using a calcium ionophore, ionomycin at concentration of 10 μ M(Calbiochem, La Jolla, CA) (0.0015%w/v).

Second messengers, cAMP

cAMP (Sigma Aldrich, ST. Louis MO) was added directly into the culture media at a concentration of 10 μ M. Intracellular cAMP was perturbed using three different mechanisms. Adenylyl cyclase was augmented directly by Forskolin (MP Biomedicals, Solon OH), (50 μ M)[163], and indirectly through G protein induction with isoproterenol (Sigma-Aldrich, St. Louis, MO) (10 μ M)[164]. cAMP breakdown was also inhibited by using Rolipram (MP Biomedicals, Solon, OH)(10 μ M), a phosphodiesterase type 4 inhibitor.[165] Synergistic and cAMP ceiling effects of the drugs were studied using forskolin/isoproterenol, rolipram/isoproterenol, and rolipram/forskolin in combination.

Junctional complex disruption (tight junctions), Protamine

Protamine (MP Biomedicals, Solon, OH) diluted in PBS (BioWhittaker, Walkersville, MD) and buffered in Krebs-Ringer (27.4 mM NaCl, 1 mM KCl, 0.2 mM MgSO₄·7H₂O, 0.06 mM KH₂PO₄, 0.06 mM NaH₂PO₄·H₂O, 2.8 mM Trizma base, 0.56 mM CaCl₂·2H₂O, and 1.8 mM glucose) was added to the culture media to a final concentration of 10 mg/ml (pH 7.4, adjusted with HCl after protamine addition).[166] The culture media bathing the monolayers were gently withdrawn

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and replaced by the buffered protamine to both the apical and basolateral compartments. The control buffer solution not containing the polycation was delivered in the same volume.

Junctional complex disruption (tight junctions), Serum free conditions

Cells were passaged onto wells containing serum free media for at least 3 days. Cell viability in serum-free conditions was first verified with qualitative assessments of growth and cell morphometry. When cells in both serum-free and serum-containing media were in confluency, TEER values were recorded and permeability measurements performed.

Junctional complex disruption (tight junctions), Dexamethasone studies

Cells were treated with dexamethasone (Sigma Aldrich, St. Louis, MO) at a concentration of 10 μ M. After 24 hrs, the permeability of cells was performed by taking measurements every hour for 8 hrs. Cells receiving the control buffer solution were measured during the same time periods. Given the potential mechanism of steroids on protein induction, the experiments were repeated 3 days after being subjected to dexamethasone. TEER was measured over 10 days at concentrations of 1, 5, and 10 μ M of dexamethasone.

Junctional complex disruption (gap junctions) 18 β -glycyrrhetic acid studies

To determine whether gap junctions contribute to the paracellular pathway, TEER and mannitol measurements were performed on cells treated with connexin disruptor, 18 β -glycyrrhetic acid (18 β -GA)(Fisher Scientific, Fair Lawn, NJ). Confluent cells were treated for 30 minutes of 20 mM 18 β -GA or vehicle. Exposure time and concentration was determined from dose and time response curves. Timing of transport studies was determined from temporal data gathered from serial TEER values measured at 5 minute intervals for 90 minutes at concentrations of 1, 5, 10, 20, and 40 mM 18- β -GA.

Results

Junctional Protein expression: Previously we have demonstrated the arachnoid phenotype in these cells. We now examined the proteins most important in the barrier development in the

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immortalized arachnoid cell line. Immunoreactivity for anti-ZO-1 and claudin indicate the presence of tight junctions. (Figure 4.1) This adds to our previous report of desmoplakin immunopositivity, indicating both desmosomal and tight junction cell-cell attachments. Tight junction proteins were marginated at edge of the cell abutting next to adjacent cells. Confluent cells in monolayers showed polygonal morphology and were cobblestone in appearance. Connexin immunopositivity indicate that gap junctions as an additional junctional structure were also present. Previous demonstrations of vimentin and cytokeratin intermediate filaments are complemented now by actin positivity which extends to junctional zones. This is in keeping with their role as intracellular link to the tight junction. (Figure 4.1)

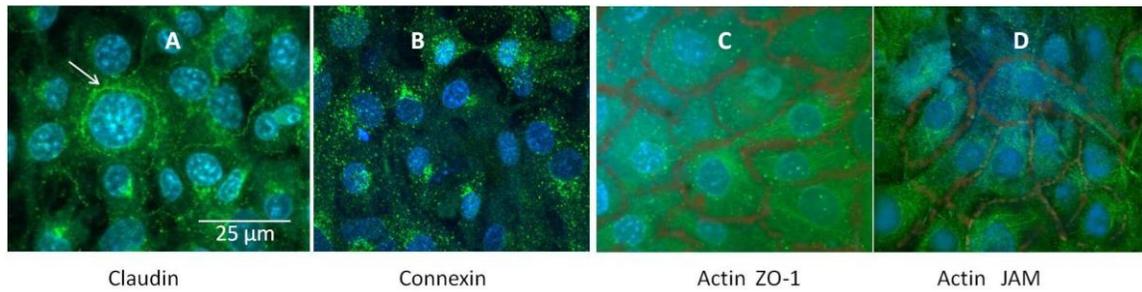


Figure 4.1: Junctional protein immunohistochemistry and actin staining. A) Immunostaining for claudin-1 (green) demonstrates the margination of the protein along the edge of the cell in contact with adjacent cell. **B)** Punctate staining (green) of connexin consistent with the presence of gap junctions. **C)** Double staining for actin and ZO-1. Filamentous appearance of actin cytoskeletal protein (green) is seen as well as the second tight junctional protein, ZO-1, along the periphery (red). **D)** JAM (red), a third component of tight junctions seen along the margin of the cell co-localizes with actin (green) intracellularly. DAPI for nuclear staining is blue on all panels. Scale is identical on all panels.

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Marker and size differential studies, A to B B to A: Mannitol, urea, and inulin were used as benchmark for paracellular transport in this arachnoid cell line.(Figure 4.2A-C) Using uncoated polyester filter with confluent monolayers, we determined first stable TEER values and consistent permeability coefficients and compared them to primary cell coefficients as well as CACO2 as control model. Monolayers of the immortalized cell lines show differential permeability to classic markers of barrier; inulin, mannitol, and urea permeabilities are $1.0 \pm .29 \times 10^{-6}$, $0.8 \pm .18 \times 10^{-6}$, $2.9 \pm 1.1 \times 10^{-6}$ cm/s (\pm indicates s.e.) respectively, which were similar to primary cell cultures. (Table 4.1) In addition, cells demonstrated size delimited differences in barrier separation when using 10-, 40-, and 70-kDa FITC-dextran as tracers. The monolayers were studied with tracers placed in the basolateral (B) side and apical (A) side. (Figure 4.2D-E) Directionality was not statistically different suggesting a non-intracellular mechanism of transport (Figure 4.2F) and is consistent with paracellular movement.

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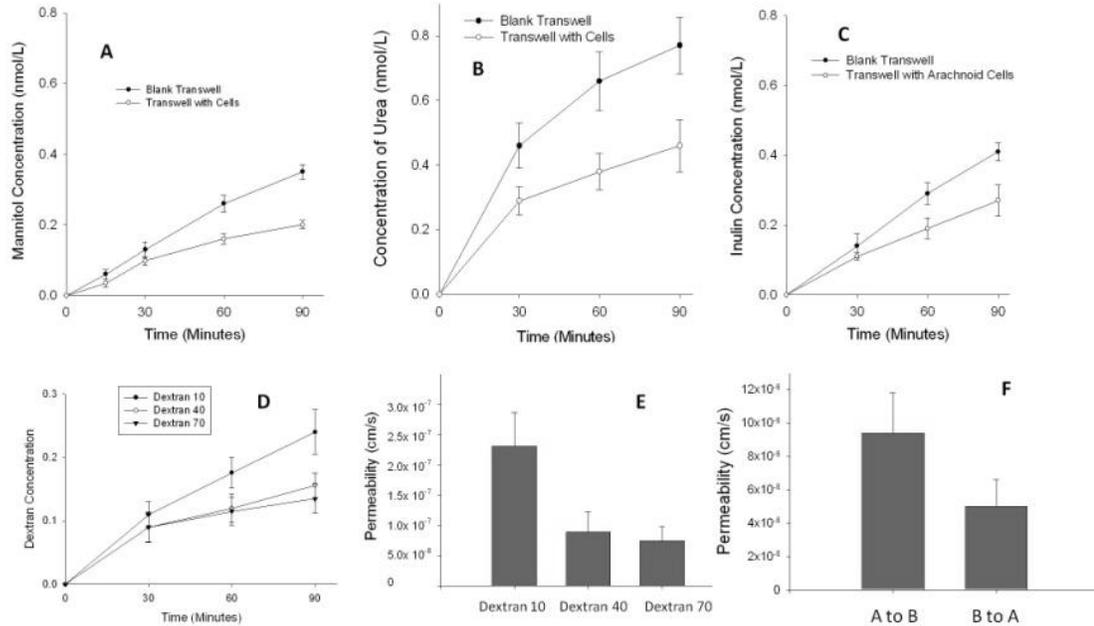


Figure 4.2: Paracellular marker and size differential studies. Permeation studies for standard paracellular tracers, A) mannitol, B) urea, C) inulin. (n=3 for each) D) Permeability curves for FITC Dextran, and E) Bar graph demonstrating steep decrease in permeability around molecular weight of 10,000. Permeability of small tracers is one order of magnitude higher than FITC-dextran 10. F) Directionality of cell line monolayer from apical to basal and basal to apical is not statistically different. Permeabilities were 5.2×10^{-6} cm/s for B to A SE 1.3 and 9.8×10^{-6} cm/s for A to B SE 2.4, paired t-test, $p=0.065$.

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Pore size and pore occupancy:

Using the Renkin hindrance function for mannitol and urea, the theoretical pore size is calculated to be 11Å and the occupancy to pore length ratio to be 0.7 to 0.8 cm⁻¹. (Table 4.1) Others have shown that anionic forms of tracers tend to have lower permeabilities than those of equivalent molecular weight in caco2 cells.[160] When using inulin, pKa of 6, permeability plateaued to the same level as mannitol. This could be due to wider paracellular space of arachnoid and the mild acidity of inulin.

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Table 4.1: Transport parameters in arachnoid cell line

	m.w.	F(r/R)	P (cm/s)	ϵ/L (cm^{-1})	D (cm^2/s)	R(\AA)	pKa
urea	60	.297	$2.9 \pm 1.1 \times 10^{-6}$.80	1.22×10^{-5} (S-E eqn*)	2.67 [167]	Neutral
mannitol	182	.125	$0.8 \pm .18 \times 10^{-6}$.72	8.9×10^{-6} (S-E eqn, [168])	4.10 [167]	Neutral
inulin	5000-5500		$1.0 \pm .29 \times 10^{-6}$		2.9×10^{-6} (S-E eqn, [168])	15 [169] 11 [168]	6.33
FITC-Dextran 10	10,000		$2.3 \pm .56 \times 10^{-7}$		1.2×10^{-6} [170]	23 [169] 17.8 [170]	9-10
FITC-Dextran 40	40,000		$8.9 \pm 3.3 \times 10^{-8}$		$.47 \times 10^{-6}$ [170]	46 [170]	9.1
FITC-Dextran 70	70,000		$7.4 \pm 2.3 \times 10^{-8}$		$.37 \times 10^{-6}$ [170]	58 [170]	6.7

*S-E eqn = Stokes Einstein equation

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Perturbation Studies

Calcium

Calcium is known to be important in the regulation of adherens junctions and tight junctions.[171] Increasing extracellular calcium up to 10mM did not increase TEER nor permeability of mannitol. However, extracellular chelation with EDTA resulted in an increase in permeability consistent with other junctional models such as MDCK.[172](Figure 3A) Chelation effects occurred within 15 minutes of drug addition, and were dose dependent.(Figure 4.3B-C) Effects were persistent until reversal by washing the cells with normal media. Tight junction also depends on intracellular calcium as a second messenger for modulation. We used a calcium channel blocker, verapamil, which did not alter permeability of mannitol significantly. When we raise intracellular calcium stores via ionomycin, permeability increased. (Figure 4.3D) This is consistent with data that suggest tight junction formation is disrupted only by certain intracellular compartments.[173]

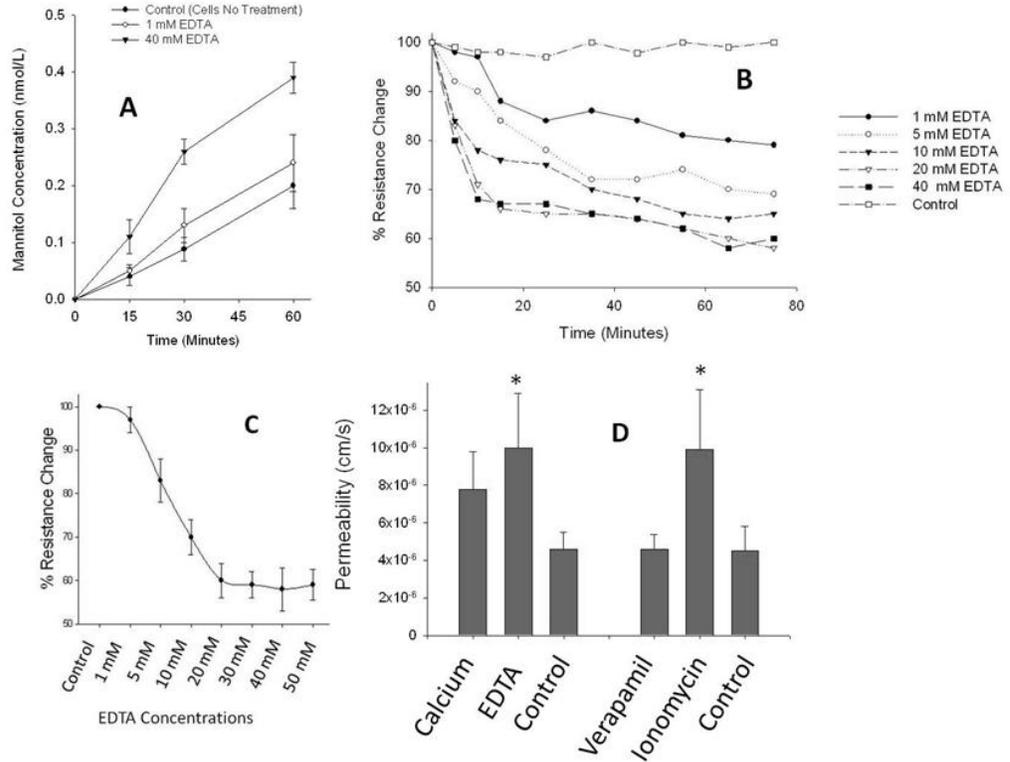


Figure 4.3: Calcium modulation of arachnoid. A) Permeability curves demonstrating differential transport of mannitol with 1mM and 40mM EDTA. B) Effect appears to begin almost immediately with maximal effect in the first 15 minutes and all dosing. C) Dose response curve showing TEER change from 1mM to 50mM. Maximal change occurs at about 20mM. D) EDTA permeability was significantly higher than control (t-test $p=0.041$). Ionomycin had similar effects on paracellular transport (data not shown) and also caused significantly higher permeabilities ($p=0.043$), while extracellular calcium and verapamil had no difference from control.

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cAMP

cAMP is known as a second messenger that prevents increased endothelial permeability under the influence of permeability augmenters.[174][175]. We looked at the role of cAMP alone on the effects on paracellular transport and did not find a change in TEER nor mannitol permeability. Rolipram, a PDE4 inhibitor, increased intracellular cAMP and caused a significant decrease in permeability. Likewise, the beta 1,2 agonist, isoproterenol decreased permeability.(Figure 4.4A) When used in combination, isoproterenol and rolipram did not cause a more marked effect nor isoproterenol and forskolin, a direct adenylyl cyclase agonist. Also, the TEER did not change. (Figure 4.4B) This may indicate a ceiling effect in the cAMP pathway. Forskolin alone and forskolin and rolipram did not induce much change in the paracellular permeability. (Figure 4.4C) Application of cAMP modifiers did not alter actin nor tight junction protein expression. (Figure 4.4D-E)

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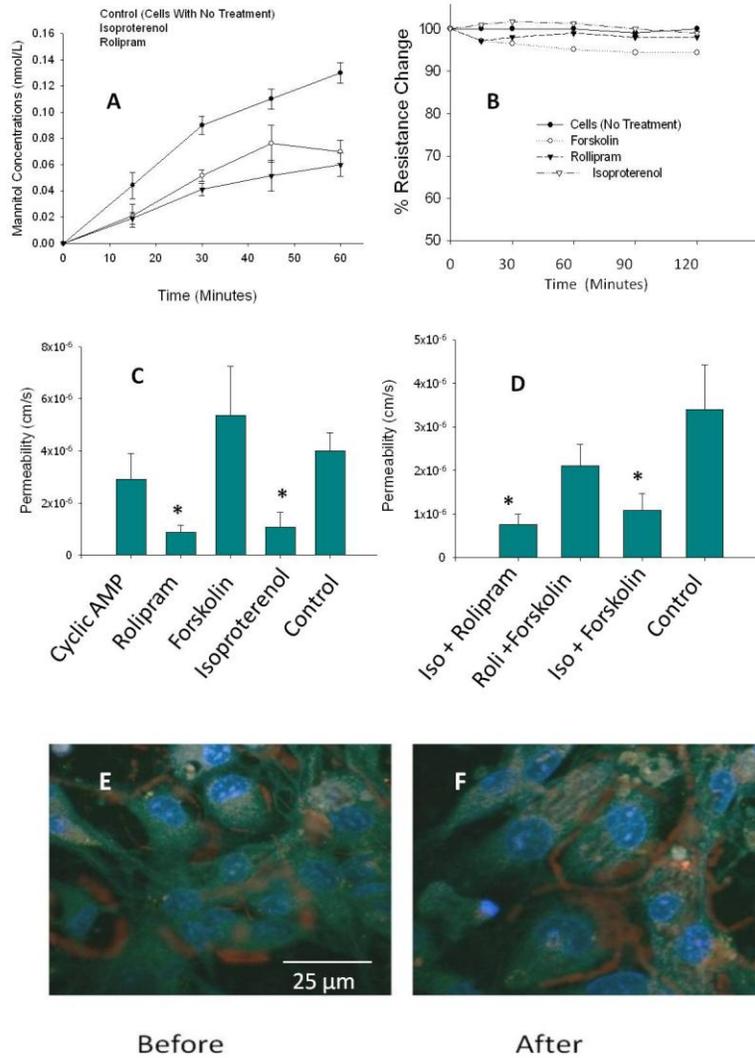


Figure 4.4: cAMP modulation of arachnoid permeability. A) Permeability curves demonstrating differential transport of mannitol with Rolipram and Isoproterenol. B) TEER showed minimal change with Forskolin (50 μM), Rolipram (10 μM) and Isoproterenol (10 μM). Experiments were carried out to 48 hours without change in the trend (data not shown). C) cAMP added into media and Forskolin induced minimal changes to mannitol permeability while Rolipram and isoproterenol decreased permeability significantly (t test, p=0.020 and

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0.024 respectively). D) When drugs were used in combination, permeability did not decrease further. E) Before and F) After addition of Isoproterenol and Rolipram, cells showed similar appearance in ZO-1 (red) and actin (green) staining.

Junctional proteins

We studied the tight junctions directly using three means and gap junctions by one. Gap junction was disrupted by 18β -GA rapidly as well in a dose dependent manner. (Figure 4.5A-C) Effect was seen within 10 minutes of drug application resulting in an approximately 3 fold increase in mannitol permeability. Serum free conditions should disrupt paracellular barrier by delocalizing the tight junction nonspecifically, while protamine affects the tight junctions by disrupting cytoskeletal attachment to the tight junctions and downregulation of claudin. Dexamethazone up-regulates claudin potentially tightening the tight junction decreasing permeability. Serum free conditions did not alter mannitol permeability despite several days of culture, nor did prolonged (days) exposure to dexamethazone. (Figure 4.5D) Protamine however significantly increases permeability within several minutes of drug application.

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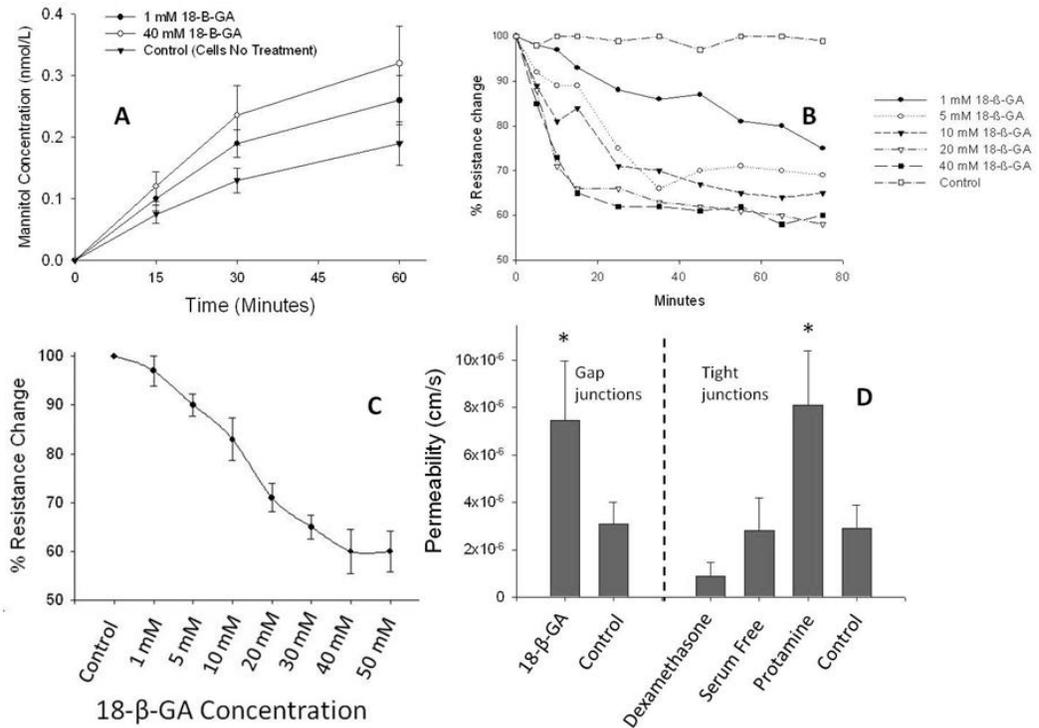


Figure 4.5: Perturbation of junctional proteins on arachnoid paracellular transport. A) 18-β-GA disrupted barrier properties of the arachnoid (t-test, $p=0.045$). Permeability curves of paracellular tracer, mannitol, altered by variable concentrations of 18-β-GA. B) Effect of 18-β-GA began almost immediately and plateaued at about 30 minutes. C) 18-β-GA appears to alter permeability in a dose response manner as manifested by TEER D) Dexamethasone, serum free conditions have minimal effect on mannitol permeability while protamine disrupted barrier formation significantly (t-test $p=0.042$).

Discussion

The barriers that surround the central nervous system are critical for its homeostasis and its protection. While the blood brain barrier has been investigated intensively, only recently has

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much attention been paid to the blood CSF barrier. Even so, the focus has been on the production side of cerebrospinal fluid, namely at the choroid plexus, but the gateway to the egress of CSF and the interface of blood to the CSF at the arachnoid granulations and membrane has largely been ignored. We have previously developed an immortalized cell line of arachnoid cell [156] and demonstrated that it forms barriers similar to monolayer models of the BBB.[154] Because of the importance of paracellular transport to the blood CSF barrier, we focus on characterizing this extracellular component of the arachnoid CSF sink. Paracellular transport is governed by a variety of mechanisms and components: cell height, paracellular space tortuosity, tight junctions, and gap junctions. Tight junctions are made up of several proteins including claudin, which is under the regulation of calcium-dependent PKC activators. The PKA pathway is important as well; cAMP activates PKA which impacts on cell-cell adhesion via RhoA inhibition. Therefore, not only are calcium and cAMP critical for routine cellular functions, but also the regulation of paracellular transport.

Paracellular Transport Studies

Dextran

Previous studies have indicated paracellular junction does not permit free passage of macromolecules of 3 nm through the interendothelial junctions[176]. If this is the case, then passage of higher molecular weight dextran should not occur. Others have demonstrated transvesicular transfer in arachnoid cells before.[36] This may compound an accurate recording of paracellular rate. In caco2 cells, macromolecules may pass through albeit with permeability coefficients two orders of magnitude smaller than standard paracellular tracers.[169] This may be due to either creation of transcellular transport or widening of the paracellular space. In order to insure that vesicular transport does not interfere with our paracellular transfer determination in the immortalized arachnoid system, the dextran was carried out over a wide geometric range and molecular weights. At approximately 10,000 daltons, the permeability began changing over an order of magnitude which clarified the mark at which the blood CSF barrier lies.

Equivalent pore size calculation

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Determination for theoretical pore size is useful in characterizing paracellular transport. It incorporates features of the paracellular space including tortuosity, gap width, cell height, lateral spaces and various junctional protein hindrances. While of limited anatomic accuracy, pore size can use charge, molecular radius, and other rate-determining physicochemical properties to help predict permeability of various substances. We first determined the validity of using this calculation by determining size limitations of the paracellular space. The Renkin hindrance equation is valid for r/R under 0.4. r/R ratio in the Renkin sieving function can exaggerate the diffusional resistance and underestimate pore radius otherwise. Using paracellular markers of neutral pKa for experimental determination would decrease solute to pore wall interactions. Our calculation of approximately 11Å indicates pore size to be larger than caco-2 cells (~5.2Å)[160].

Calcium

Calcium is a second messenger for PKC, but PKC effect on paracellular permeability is variable.[177][178] PKC activation helps assemble tight junctions but can impair established junctional integrity. [179] The PKC α isoform mediates disassembly via actin mediated cell contraction and is calcium and DAG-dependent.[180][181][182] PKC β , also calcium and DAG-dependent, increases endothelial permeability [183] as indicated by PKC beta 1 gene transfer in a microvascular endothelial cell line. [184] Intracellular calcium is considered a key regulator in cell contraction and junctional disassembly [185][186] and is increased with release from endoplasmic reticulum stores.[187] Tight junction modulation by intracellular calcium may also proceed via alterations in the subcellular localization of occludin[188]. We found that the addition of calcium to the extracellular solution did not change arachnoid cell permeability. Furthermore, blocking calcium from entering the cell also did not change cell behavior. This supports the claim that some other compartment such as endoplasmic reticulum stores may be the key to permeability regulation. By disrupting the extracellular/intracellular calcium homeostasis via calcium ion channel drug, we demonstrated that calcium plays an active role in paracellular transport.

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EDTA was added as a chelator of extracellular calcium. This does not alter ZO-1/actin interactions unlike intracellular calcium, but may affect the cadherin-cadherin linkage via their extracellular domain.[189] Adherens junctions composed of cadherin join homotypically to adjacent cells and are calcium dependent.[176] Via p120-catenin, cadherin furthermore links the adherens junction to the actin cytoskeleton. In the arachnoid cells, the TEER values were decreased by EDTA but not by intracellular calcium manipulations, suggesting that adherens junctions may have an important role in the arachnoid barrier formation.

cAMP

cAMP prevents permeability increases by several mediators [175][174] By itself we did not see any change in TEER nor paracellular transport. When we inhibited its breakdown and directly affect adenylyl cyclase activity, we increased the barrier capability of the arachnoid. cAMP induces protein kinase A which inhibits RhoA activation and cellular contraction.[190] It may have a direct effect on actin rearrangement thereby affect intercellular space formation.[190] In addition, it can directly activate Epac, a Rap1GEF which enhances VE-cadherin junctional integrity and actin reorganization [191]. When we examined the immunohistologic staining of the arachnoid cell for actin and ZO-1 before and after the application of cAMP modulators, we did not see any gross changes in intensity or variation in staining pattern (Figure 4.4E and F). It is possible that the effect is too subtle to be detected in this manner. Other investigators have noted that cAMP's effect is most marked when the drugs were used in combination with other agents in the case for human and bovine brain endothelial cells.[192] When Rubin et al. used combination of astrocyte cultured media and cAMP, the cAMP permeability response was the greatest. The reason is not completely clear, but we intend to use astrocytic and neuronally derived soluble factors in combination with cAMP agonist as the next step in this second messenger system analysis. Even without direct contact by these supporting cells in the BCB, it is possible that they may still influence barrier behavior at the arachnoidal level.

TEER is often viewed as a marker for monolayer integrity or barrier tightness. However, its relation to paracellular permeability did not correlate in the cAMP studies (Figure 4.4). This phenomenon has been seen in other monolayer models such as the caco-2 cell line.[193][194]

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The physiology is not clear; however, it may be that the paracellular space may widen without change in the junctional protein complex structure allowing for this disparity.

cAMP and Ca second messenger systems may not be separate in their control of extracellular transport. Schmidt et al. showed a new calcium signaling pathway that is triggered by cAMP. This pathway is PKA independent and is mediated by a Rap family GTPase.[174] The receptor studied by that group was the adenylyl cyclase-coupled beta2-adrenoceptor; we used isoproterenol, a beta1,2 agonist which showed a modest effect on permeability.

Tight junction importance

Our attempt at direct alterations of the tight junction resulted in variable changes in paracellular tracer permeabilities. Steroid, an upregulator of claudin in other barrier models caused marginal effects on paracellular permeability. It is possible that we are seeing a ceiling effect due to limitations of other components in tight junction that prevent increases in barrier properties. When we used serum free conditions, very little change in permeability resulted as well. When serum is withdrawn from culture media, TEER in cerebral capillary endothelial cells increases, probably due to nonspecific re-organization of the tight junctions.[195] We found that protamine, which disrupt cytoskeletal actin distribution and decrease claudin, occludin, and potentially ZO-1 expression, to exert the most effect on paracellular barrier. Because of the polycationic nature of protamine, its action on the tight junction is nonspecific.[196] Together, evidence suggests that tight junctions by themselves in arachnoid may not be the only important component to the barrier formation. 18 β -glycyrrhetic acid, which binds on connexin at the gap junction had a profound effect on the paracellular permeability in arachnoid. Whether the cause is a mechanical disruption due to separation of the gap junction, or whether there is a loss of cell-cell communication, i.e. calcium transfer, is unknown.

Conclusion

We show that arachnoid cells have the molecular hardware and the capability to support paracellular transport. Presence of occludin, claudin-1, JAM, and actin cytoskeletal protein are

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present in these cells and play a variable role in transport. The theoretical pore size representing the paracellular space indicates that the gap is wider than vascular endothelial cells of the brain. Permeabilities for urea, mannitol and inulin are similar to other models of brain barriers and the size differentiated transport of dextran clarified the previously known blockade for soluble dye in the blood CSF barrier at the arachnoid sink. Furthermore, the dextran study indicates that in a standard membrane delimited diffusion system, the efficiency of intracellular transport is approximately two orders of magnitude less efficient than paracellular means. We also show that paracellular transport may be under the influence of both gap junction and tight junctions, and the calcium and cAMP second messenger systems influence this system. Intracellular and extracellular calcium appear to have differential roles in increasing paracellular permeability, and cAMP, likely by a variety of mechanisms, is able to decrease paracellular permeability. We therefore propose that the arachnoid transport of cerebrospinal fluid is served by the paracellular route and is influenced by a complex system of control.

Chapter 5

Chapter 5: Summary and Future Studies

Chapter 5

This thesis presents some of the foundational work for the tissue engineering of arachnoidal tissue. It illustrates the ability for three dimensional construction of a bioengineered arachnoid product, presents two cell lines as research substrates for future work, and characterizes the major characteristic of the blood CSF barrier at the arachnoid, namely paracellular transport. Compared to the literature in endothelial cells or tissue engineering endeavors in blood vessel replacement, very little has been published in arachnoid cells and granulations. Only in the past five to ten years have suitable ex vivo models been developed. The arachnoid is morphologically and ontogenetically variable. It has to serve a variety of roles, and its end form must be adapted for these roles. Therefore, we have to be flexible in constructing a variety of biomimetic products with divergent geometries and properties.

Among the three dimensional architectures that exist for arachnoid, the most complex is likely the central core. Abutting the arachnoid cap and merging into the arachnoid membrane, it forms the first barrier in the granulation to substances before they proceed to the cap and pass to the vascular system. Its reticulated structure is similar to collagen scaffolds created using lyophilization methods, and thus chapter 2 is devoted to this technique. With pore size and overall dimensions similar to the core, these scaffolds were seeded with arachnoid cells and cultured. The results were compared with two dimensional cultures morphometrically and immunohistochemically. The cell's growth characteristics were also documented. Findings were that the cells retained their arachnoid phenotype and geometrically appeared similar to native tissue. The cells populated the scaffold sparsely, which was similar to the native state as well. This was in contrast to cells grown two dimensionally ex vivo.

A lack of suitable substrate for investigation has slowed the advancement in studying arachnoid physiology. To address this issue, two new cell lines of arachnoid cells were developed in chapter 3. Using singly and doubly transduced cells with SV40LgT and hTERT, the cells were immortalized and preserved. Colonies chosen showed clear integration of the gene. Only one other attempt at transformation has been made. In the early 1990's this attempt has resulted in cells that senesced after fifty passages. The two new cell lines we created remain robust much long and are the only cell lines of arachnoid currently in existence. Not only were the growth characteristics of the cells exceptional, the immunohistochemical phenotype imitated the native

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tissue. The chapter briefly discussed the physiologic properties of the cells, preliminarily demonstrating its transport properties similarity to another border cell, the caco-2 model, to be later described in greater detail in chapter 4.

In chapter 4, the paracellular mechanisms of the immortalized arachnoid cell line was outlined using paracellular and size differentiated tracers. Classic permeability studies delineate passage of small sugars and variable size dextran through membrane supported monolayers for paracellular transport studies. The latter clarifies the size differentiated set point for the barrier limit. Theoretical pore size and occupancy to length ratio allow comparison of arachnoid to other models of blood brain barriers. Fundamental work for second messenger involvement in barrier regulation was performed, particularly for calcium and cAMP, with the goal that in the future, specific intracellular stations at the various modulatory pathways could be leveraged for transport alterations.

In total, the data gathered in chapters 2, 3, and 4 demonstrates the feasibility of the tissue engineering of an arachnoid granulation and set the stage for future study for arachnoid physiology. At the same time, large knowledge gaps become obvious and provide direction for future work. These areas include the imitation of the arachnoid cap, intracellular transport mechanisms of the arachnoid cell, carrier mediated transport in arachnoid, application of arachnoid physiology to pathologic conditions, and extension of arachnoid models to humans and other animal for better fidelity of cellular behavior. For example, the bioengineered arachnoid cap for example is distinct from the core; a dense cellular construct is needed, with minimal extracellular space. We have been able to generate such an architecture using collagen gel as a medium for cell growth but continued characterization must be preformed. Once created, the arachnoid cap must be able to integrate with the arachnoid core and blend into the arachnoid membrane. This interfacial integration may be an engineering challenge. Furthermore, it is likely the transport characteristics of the arachnoid cap would be very different from the arachnoid core. Given the higher density of cells, intracellular transport and stacked geometries of the cells may become important.

Chapter 4 defines some of the limits of paracellular transport, but intracellular transport could be important as well. For example, the passage of anti-epileptic medication through the BBB is

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dependent of transporter systems along the vascular endothelium. Likewise, cancer pharmaceuticals leverage the ABC transporter family to overcome the low brain drug concentrations. No transporter literature exists for arachnoid. Furthermore, very limited is known about aquaporins in the arachnoid. Given the importance of water removal by arachnoid *in vivo*, the role of these channels needs to be defined.

Hydrocephalus is a disease that could directly benefit from the analysis of water movement from the brain. In this condition, the removal of cerebrospinal fluid is slowed so that pressure building up within the intracranial cavity adversely affects the brain. Tissue engineering of the arachnoid granulation would be a natural substitute for the current treatment of artificial shunts that is prone to infection, breakage, and failure. Tissue engineering CSF gateways is still at its infancy. For example, can the cells lay a strong enough extracellular matrix to withstand the wide swings of intracranial pressure? How can we make the scaffolds stronger? The surgical implantation of such a device may be one of the biggest forthcoming hurdles. As the device must rest at the vascular interface directly connecting the intracranial cavity filled with the delicate neural structures to blood vessels, any small breaches in continuity would result in potentially severe bleeding complications.

Different diseases pose other challenging problems. Neurotrauma results in a host of pathologic conditions and complications. Debris from the brain, chemicals resulting from residuals of foreign material, and blood itself incite a variety of pathways that could be detrimental to the nervous system. The breakdown products of blood for example result in a plethora of oxidative pathways that could incite brain damage and prevent healing. Understanding the clearing mechanisms of the brain may lead to more rapid recovery and restoration of neural function. Clearance occurs by many mechanisms among which are the transcytosis of blood byproducts, engulfment by leukocytes, and paracellular transport of smaller molecules. Transient breakdown of the blood brain barrier and the role of indigenous phagocytic cells such as microglia contribute to the complicated routes of debris removal, but the blood CSF barrier is the one currently most leveraged by neurosurgeons. Studying the mechanisms of debris removal in neurotrauma would be a productive avenue for research in neurotransport, as potential therapeutic intervention may directly result from knowledge gained.

Chapter 5

In summary, this dissertation lays some of the foundational work for arachnoidal engineering. Much still needs to be done. Disease directed research may lead to rapid therapeutic intervention, and basic science work may lead to a more complete understanding of material egress from the brain.

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